

Independent Component Analysis of Electrophysiological Data



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Zakopane, Poland

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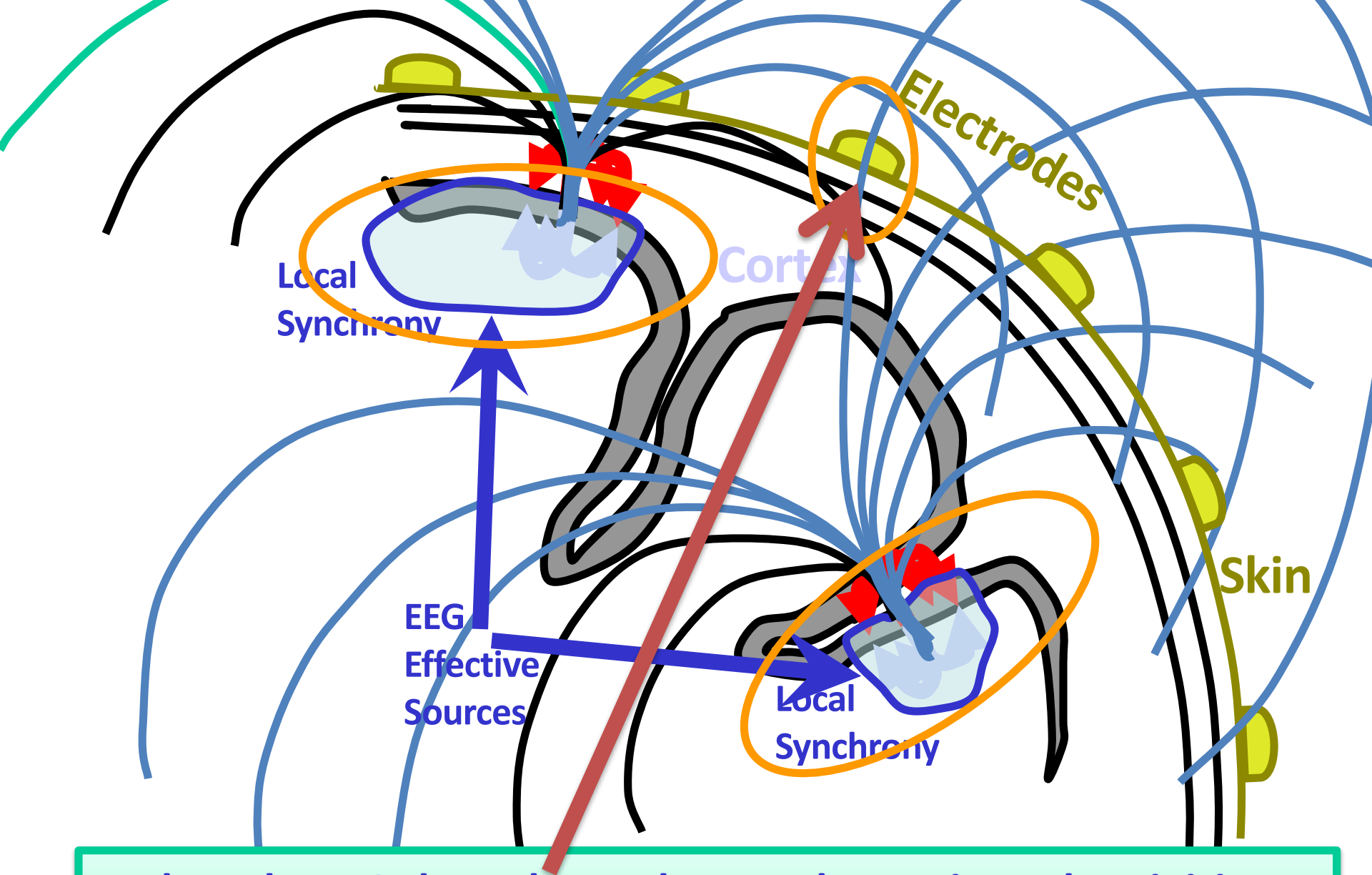


The EEGLAB environment

(sccn.ucsd.edu/eeglab)

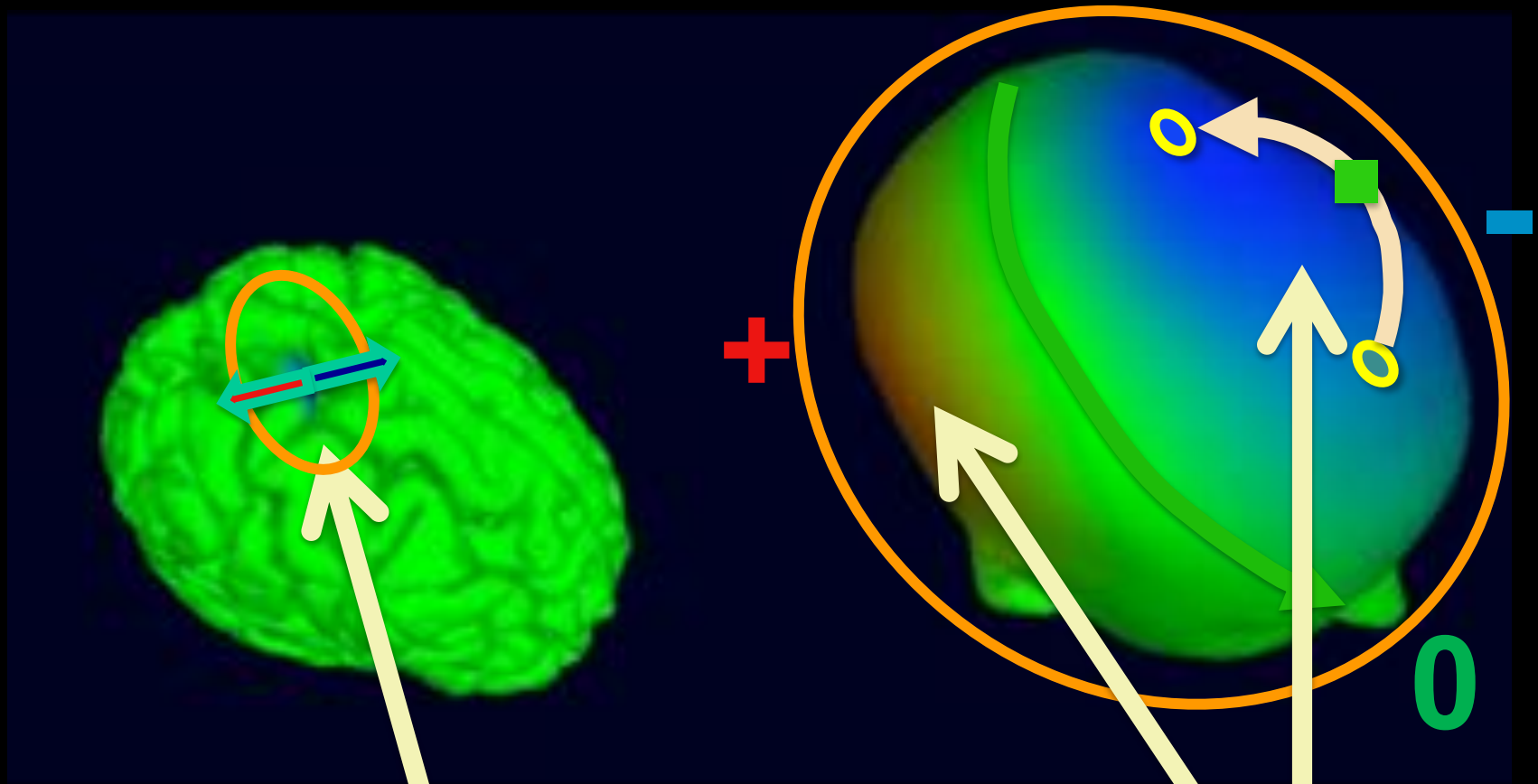
**is now available in the
Neuroscience Gateway
(NSGportal.org)**

**... In future, optional
NSG computation of EEGLAB
pipelines will be available directly
via the EEGLAB menu itself**



Each scalp EEG data channel sums the projected activities of multiple brain (and non-brain) source processes.

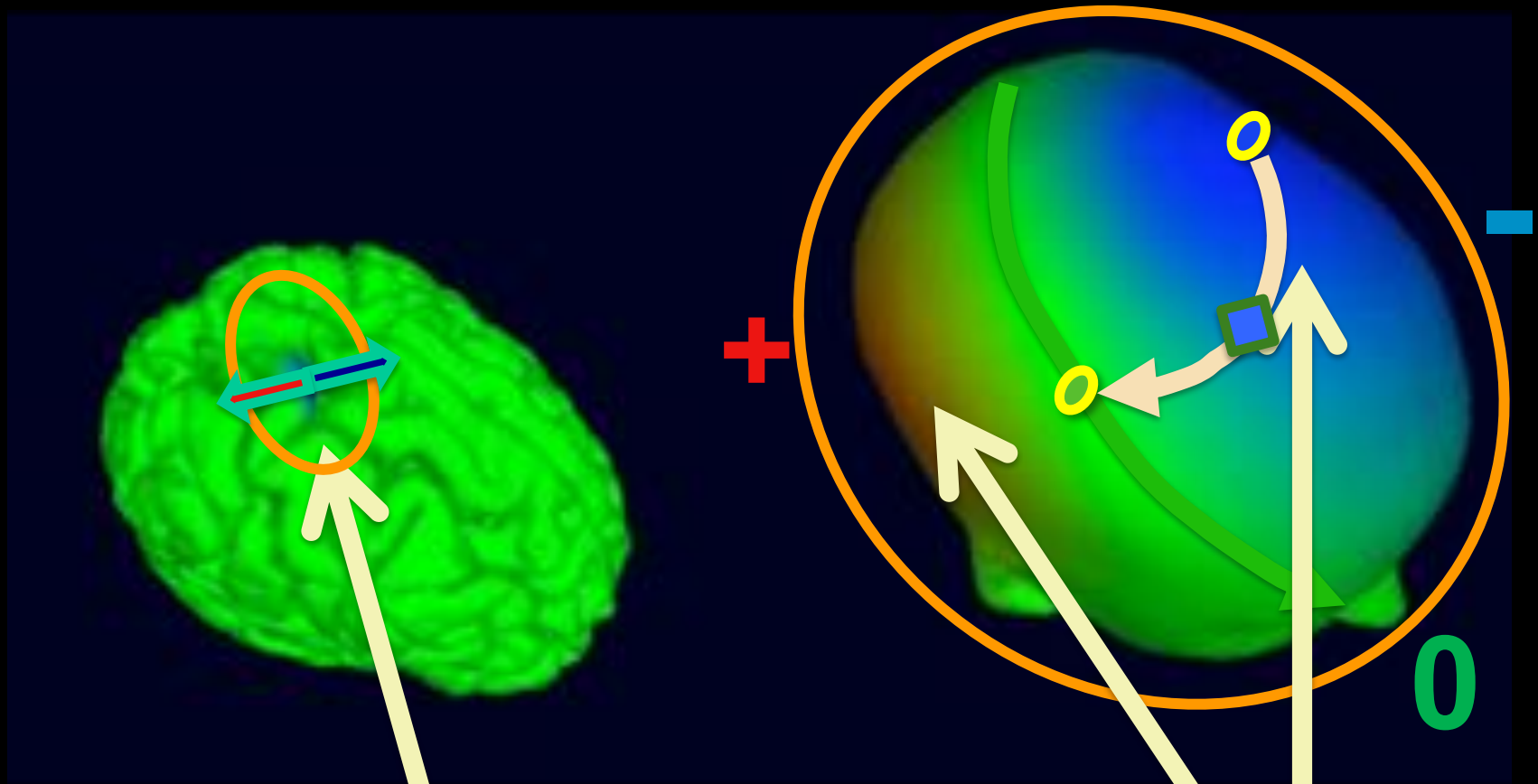
The very broad EEG point-spread function



Single simulated parietal source →

Very broad projected scalp potentials

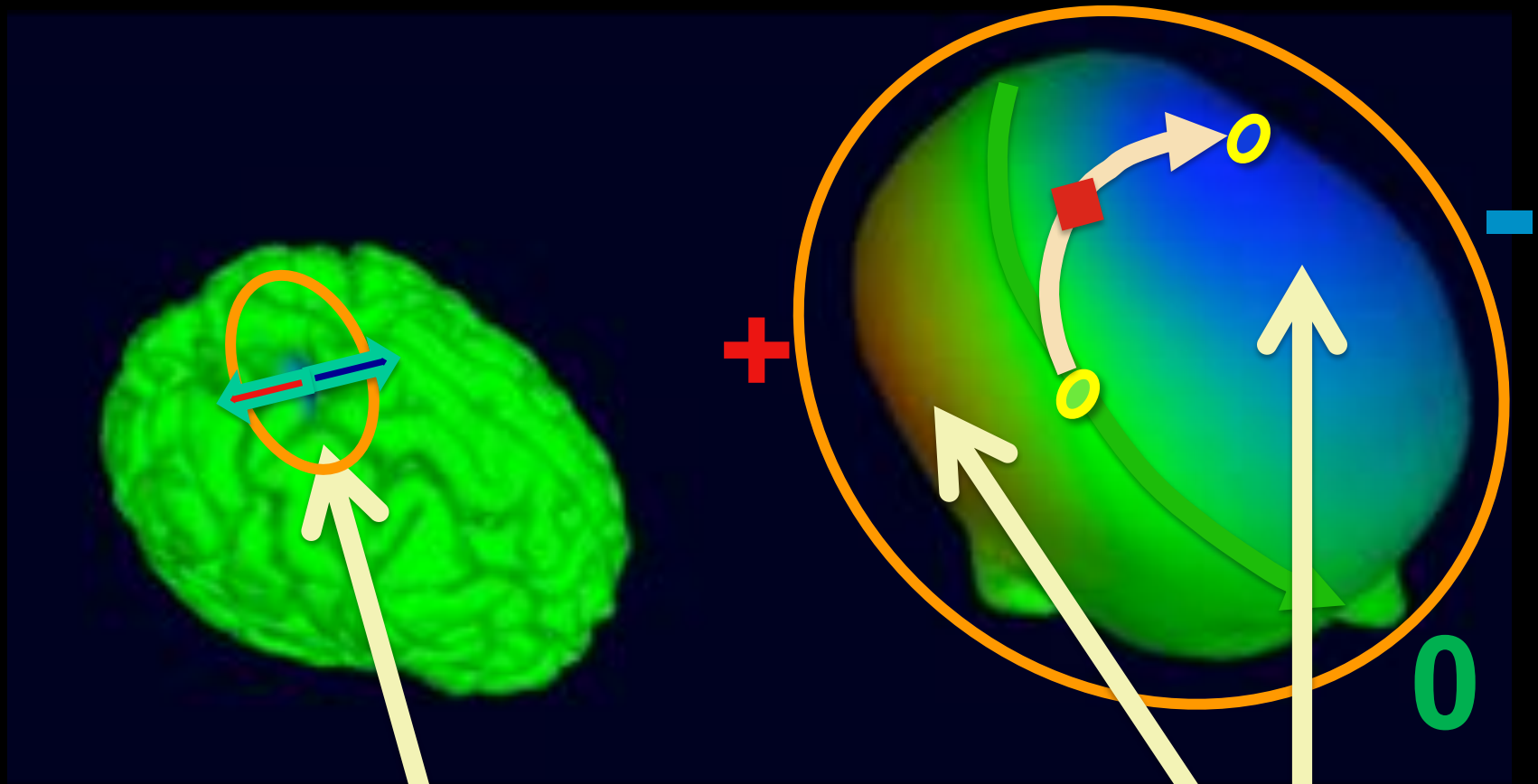
The very broad EEG point-spread function



Single simulated parietal source →

Very broad projected scalp potentials

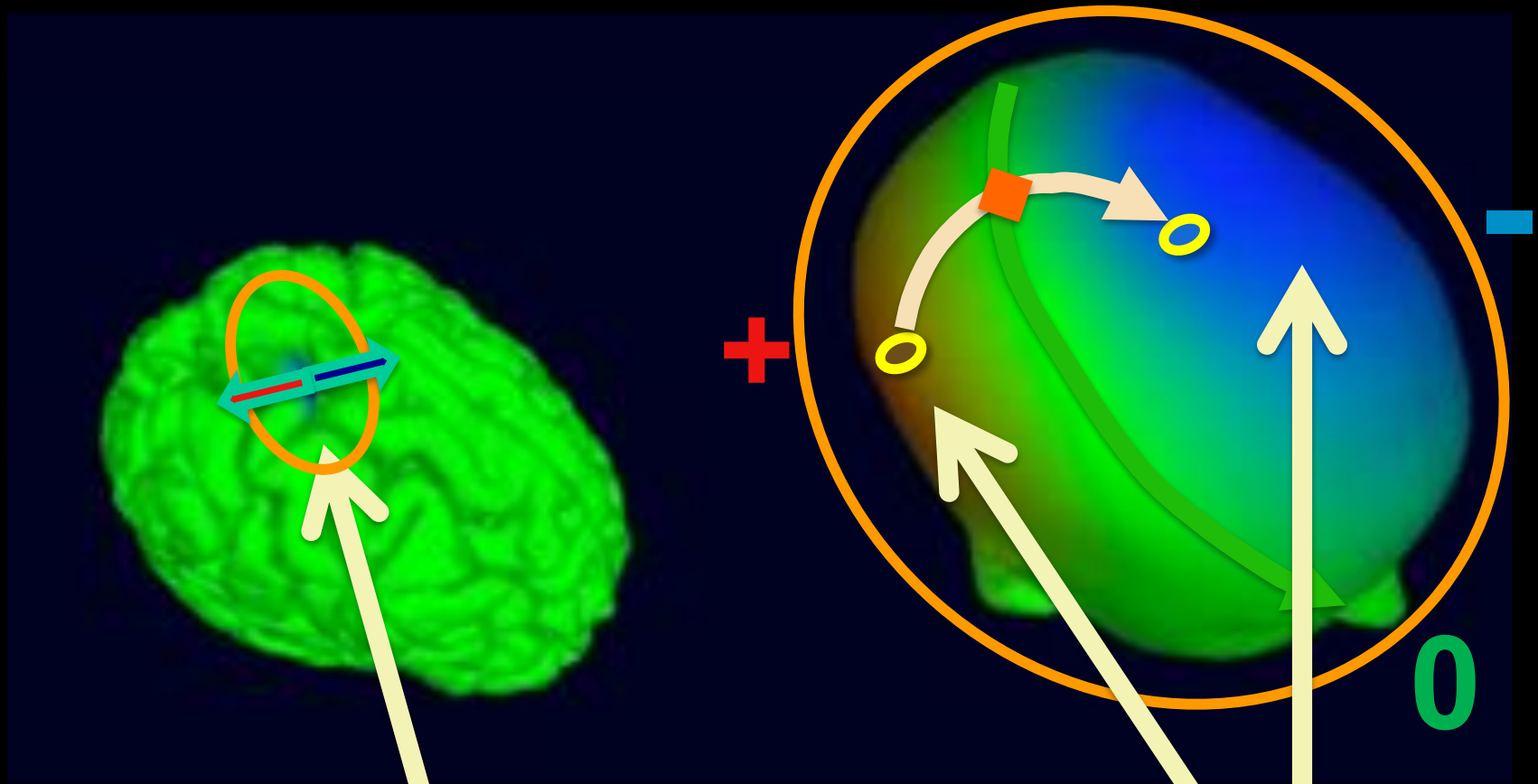
The very broad EEG point-spread function



Single simulated parietal source →

Very broad projected scalp potentials

The very broad EEG point-spread function



Single simulated parietal source →

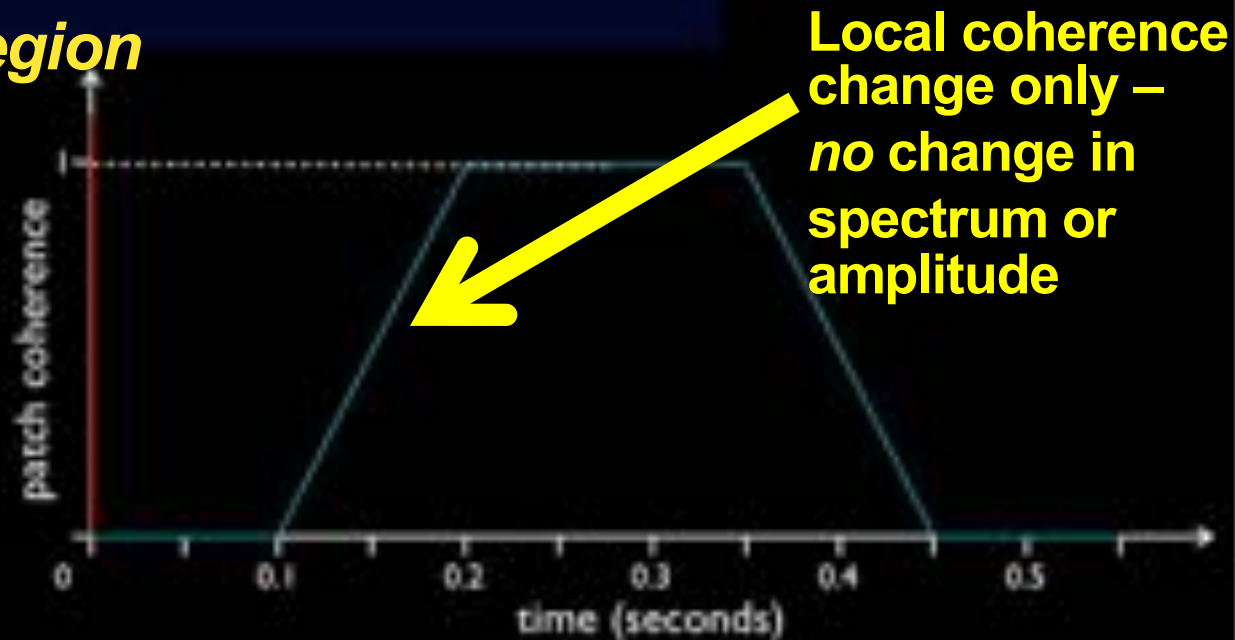
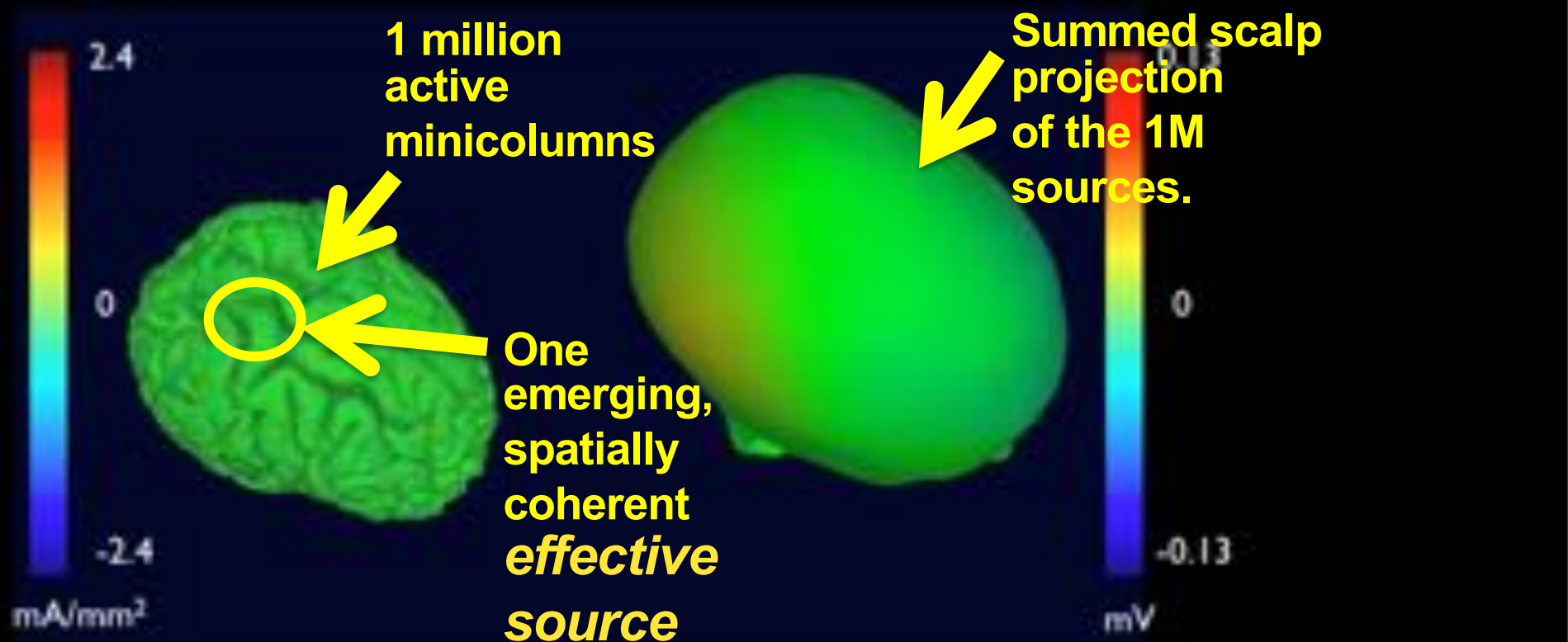
Very broad projected scalp potentials

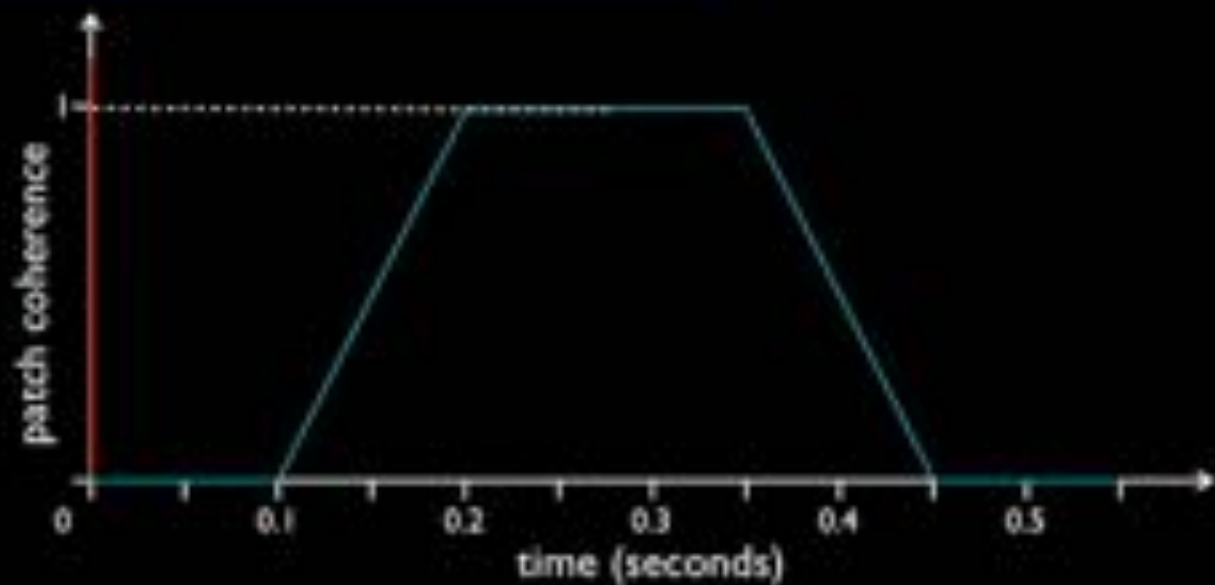
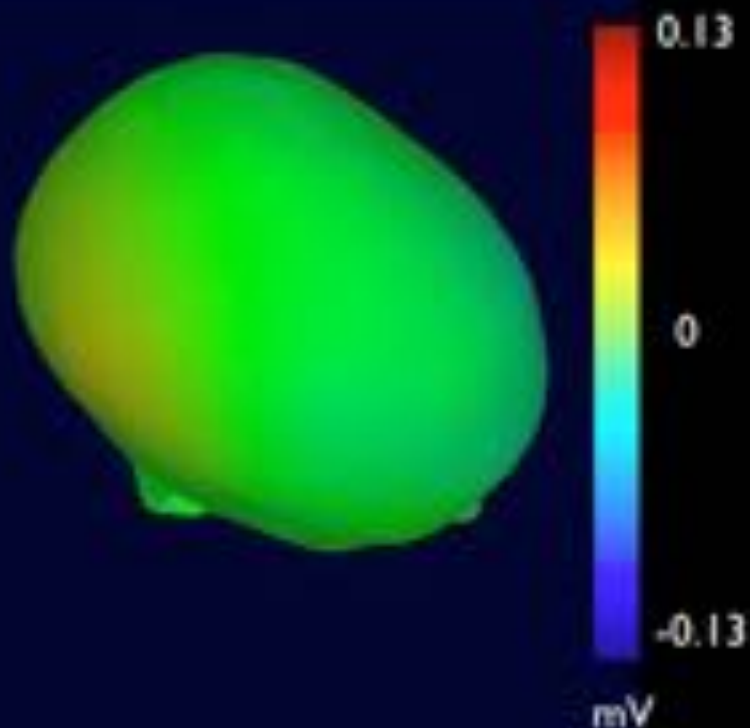
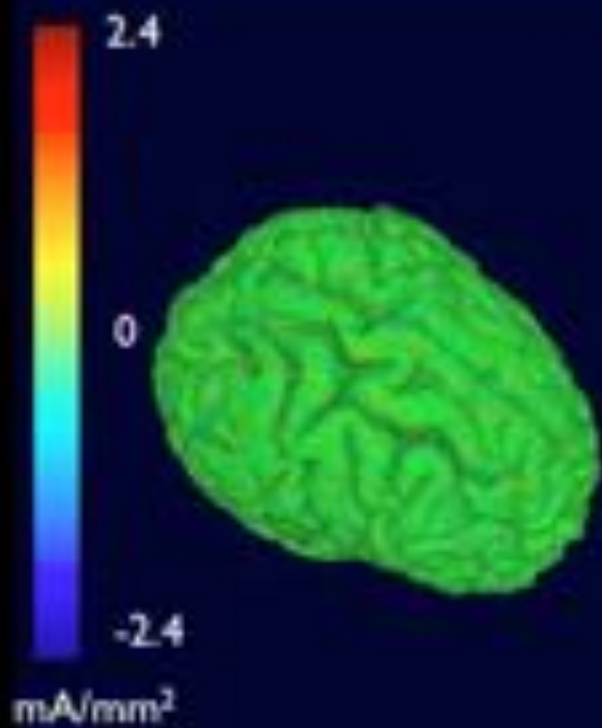
The very broad EEG point-spread function

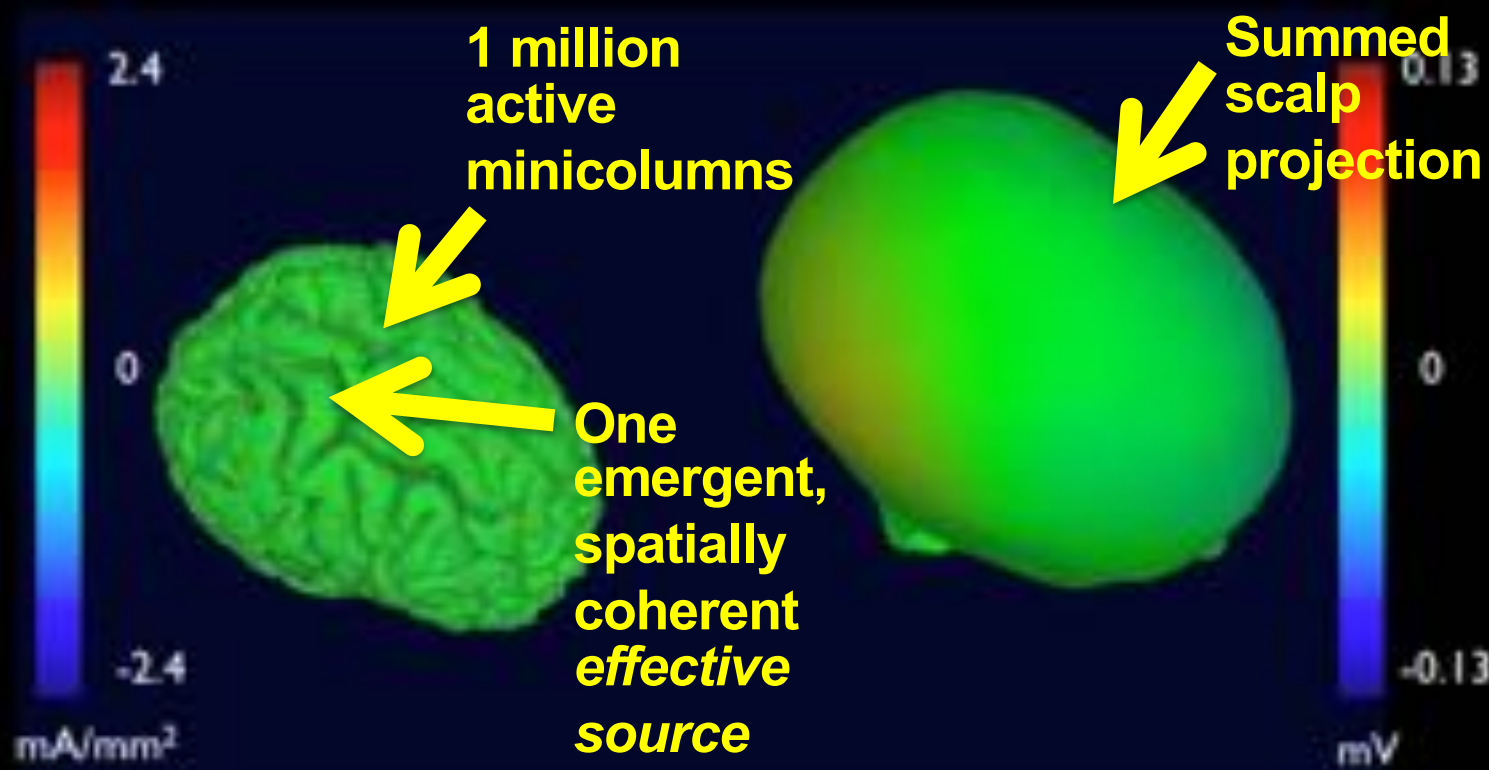
Each EEG channel records variations in a *double-ended voltage difference between (at least) two electrodes*

Each EEG channel thereby constitutes a *particular spatial filter* receptive to sources located all over the brain surface – but particularly receptive to a *complex distribution* of cortical areas – *NOT* only to one radially oriented bit of cortex located directly below *one* of the *two* (or more) channel electrodes!

Single simulated parietal source → Very broad projected scalp potentials



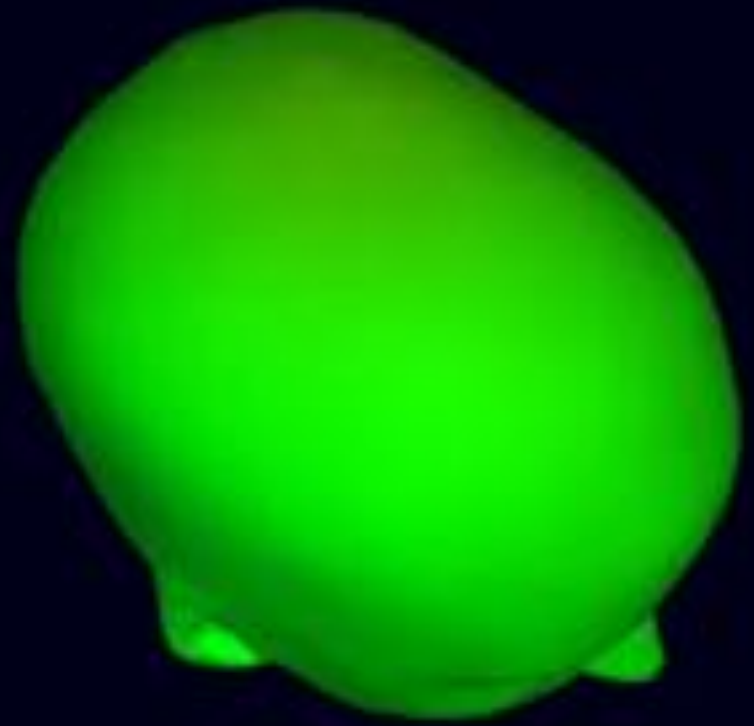
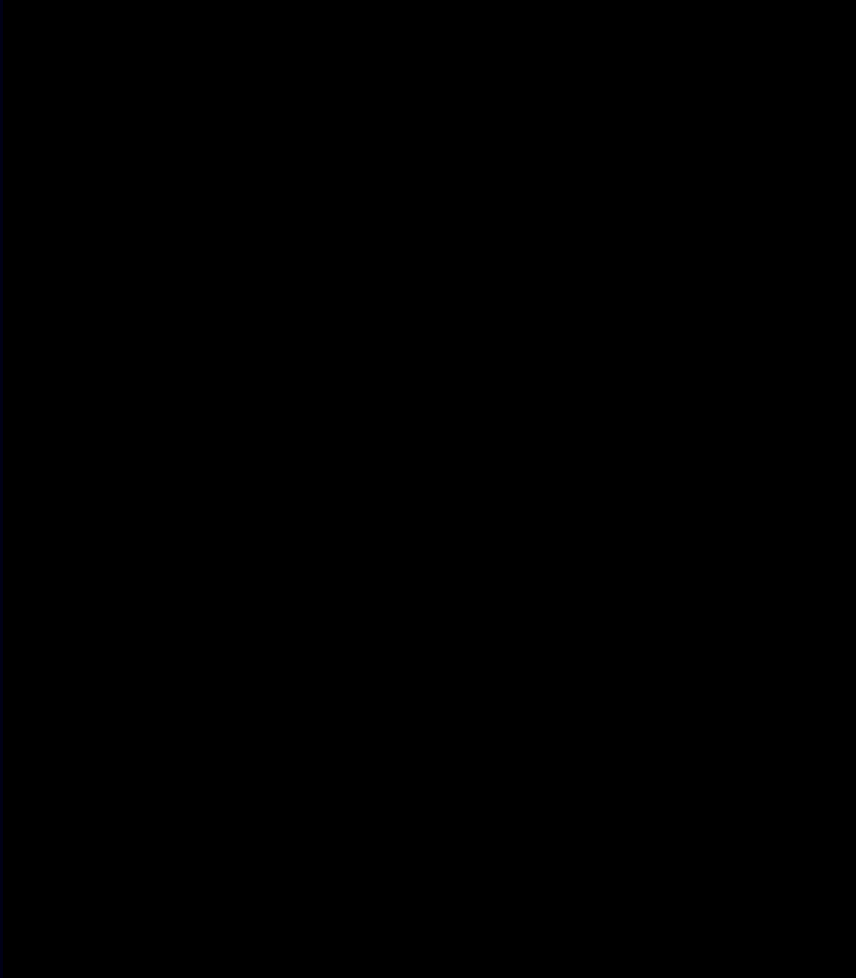




The *effective sources* of the scalp EEG are emergent islands of cortical LFP synchrony or near synchrony.



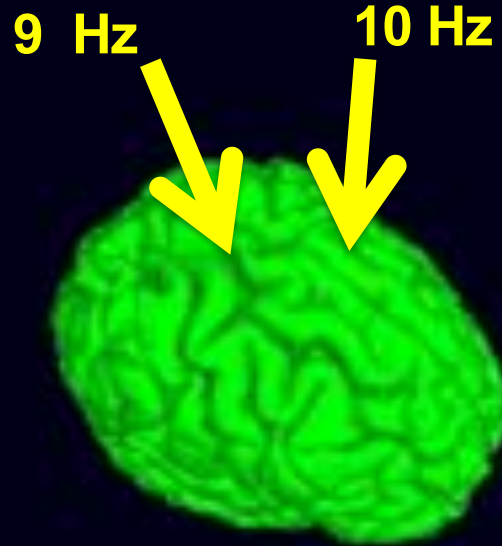
Scalp epiphenomena !



Scalp projection

Scalp epiphenomena !

Phenomena



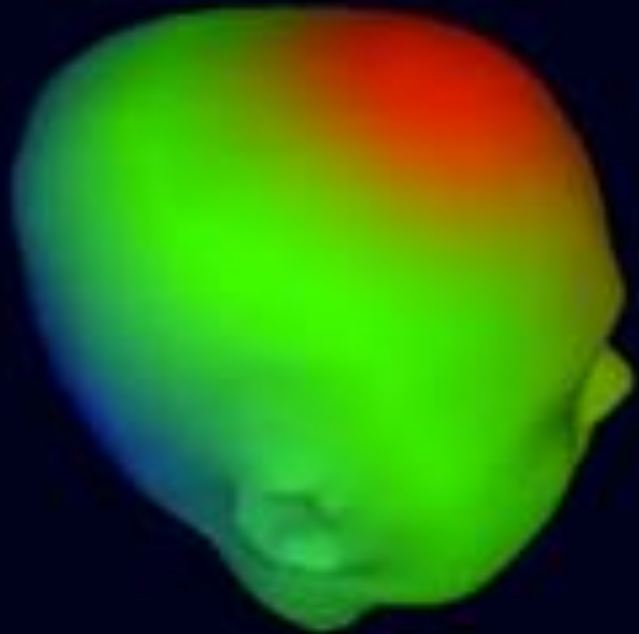
Two spatially stationary
cortical effective sources

Epiphenomenal

epiphenomena --
secondary effects or
byproducts that arise from but
do not causally influence a
process.

Summed
scalp projection

Summed scalp projections of 13 effective brain sources

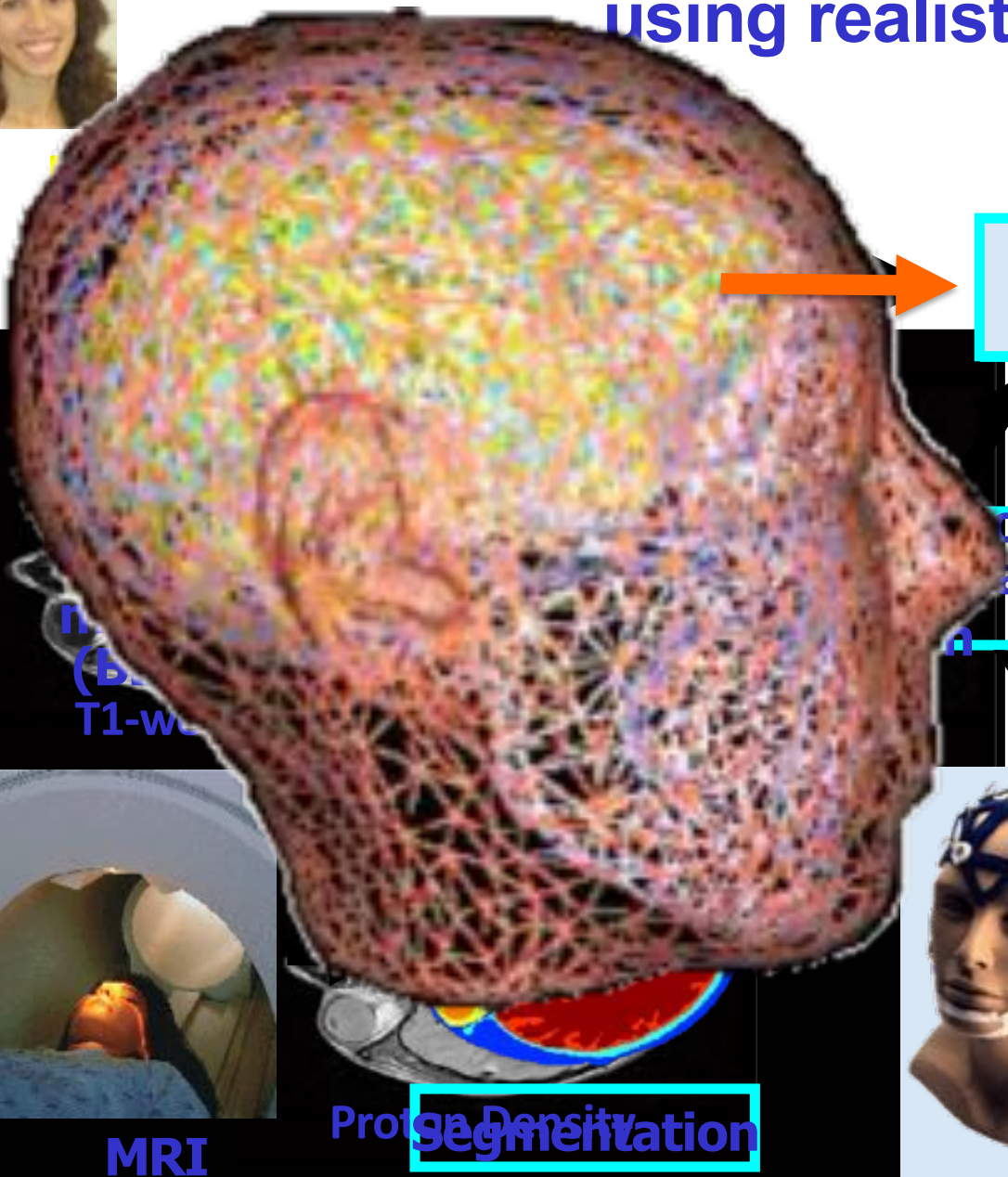


Epiphenomenal Impressions

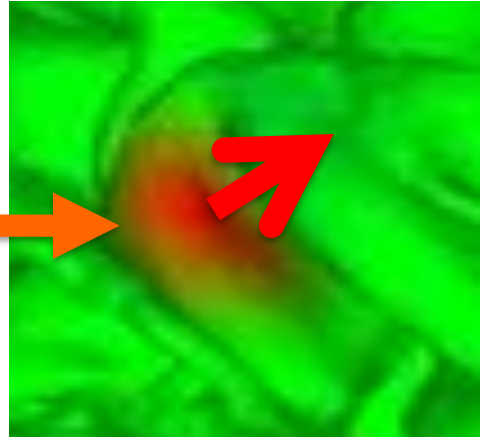


Causal Phenomena

Electromagnetic source localization using realistic head models



Simple Map



Registration

Signal Processing

Source Estimate



MRI

Proton Density segmentation



EEG/MEG

A blurred hallway with a red carpet and a large question mark in the background. The text is overlaid on the image.

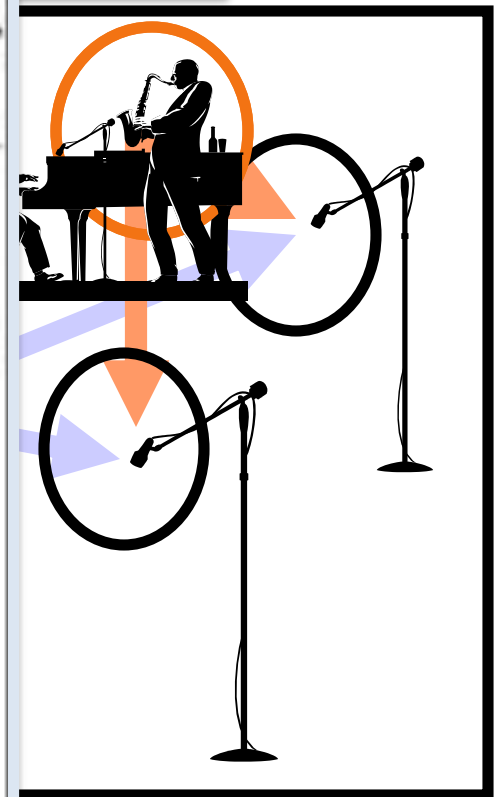
**But how to find
EEG effective sources?**

Blind EEG Source Separation by Independent Component Analysis



Tony Bell,
developer
of Infomax
ICA

ICA can find distinct EEG source activities -- and their 'simple' scalp maps!



Infomax ICA learning approach

How to make the outputs statistical independent?

Minimize their redundancy or mutual information.

Consider the joint entropy of two components,

$$H(y_1, y_2) = H(y_1) + H(y_2) - I(y_1, y_2).$$

Maximizing $H(y_1, y_2)$

minimizing $I(y_1, y_2)$.

Infomax

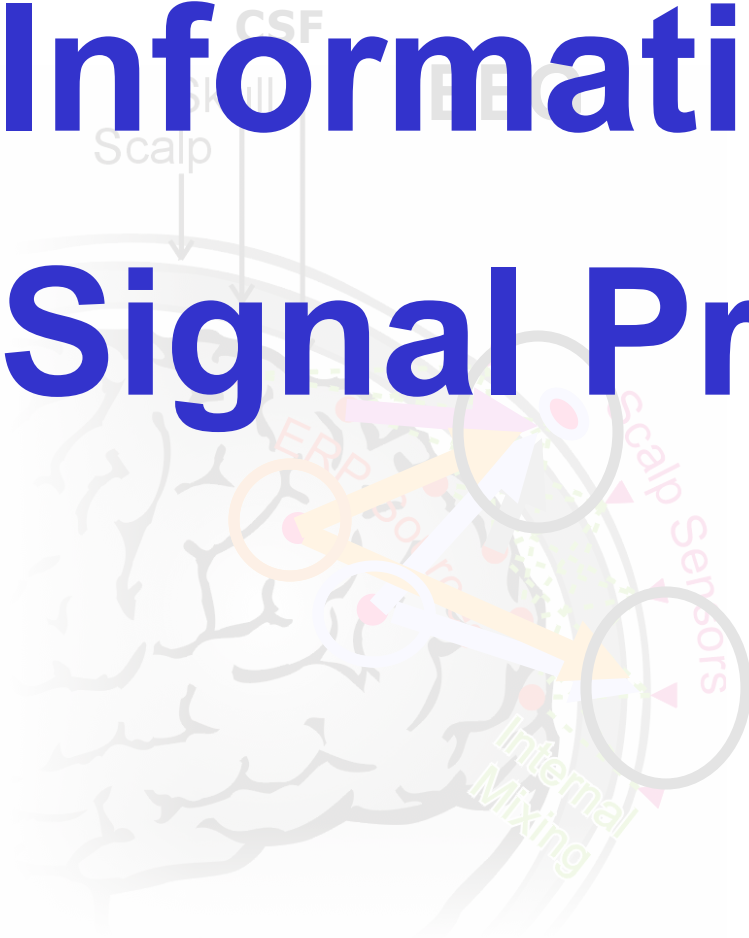
The learning rule:

$$\Delta \mathbf{W} \propto \frac{\partial H(\mathbf{y})}{\partial \mathbf{W}} \underbrace{\mathbf{W}^T \mathbf{W}}_{\text{Natural gradient normalization (Amari)}}$$

Is 0 if the two variables are independent

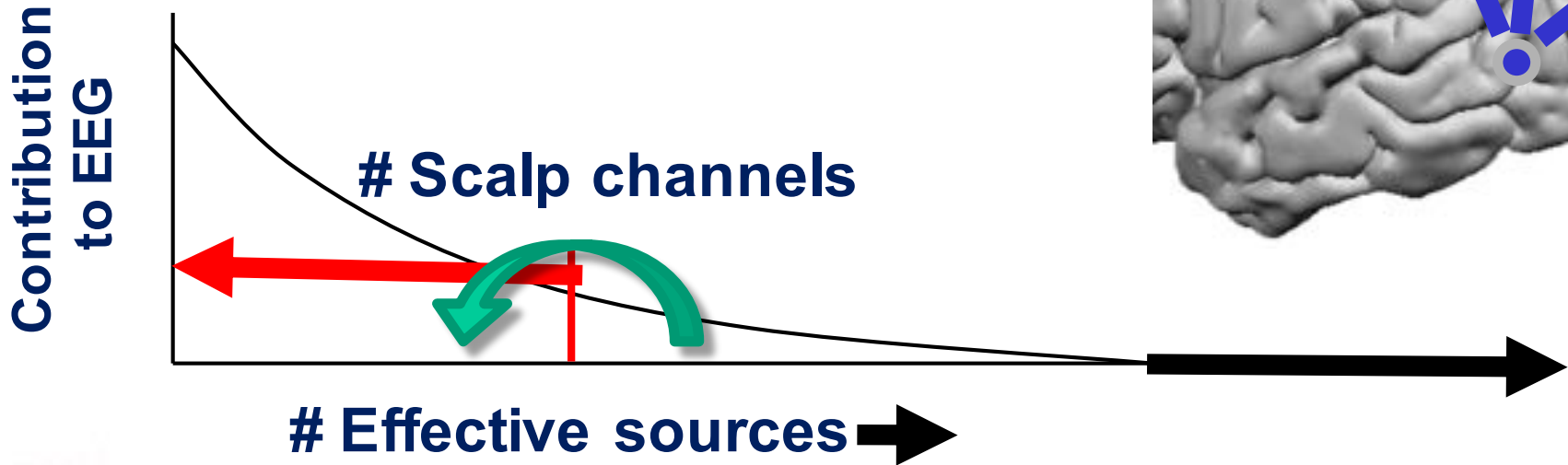
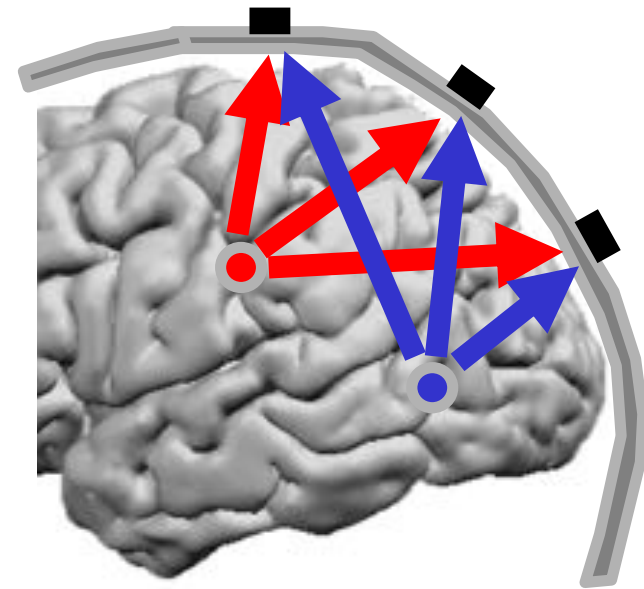
Blind EEG Source Separation by ICA

Information-based Signal Processing



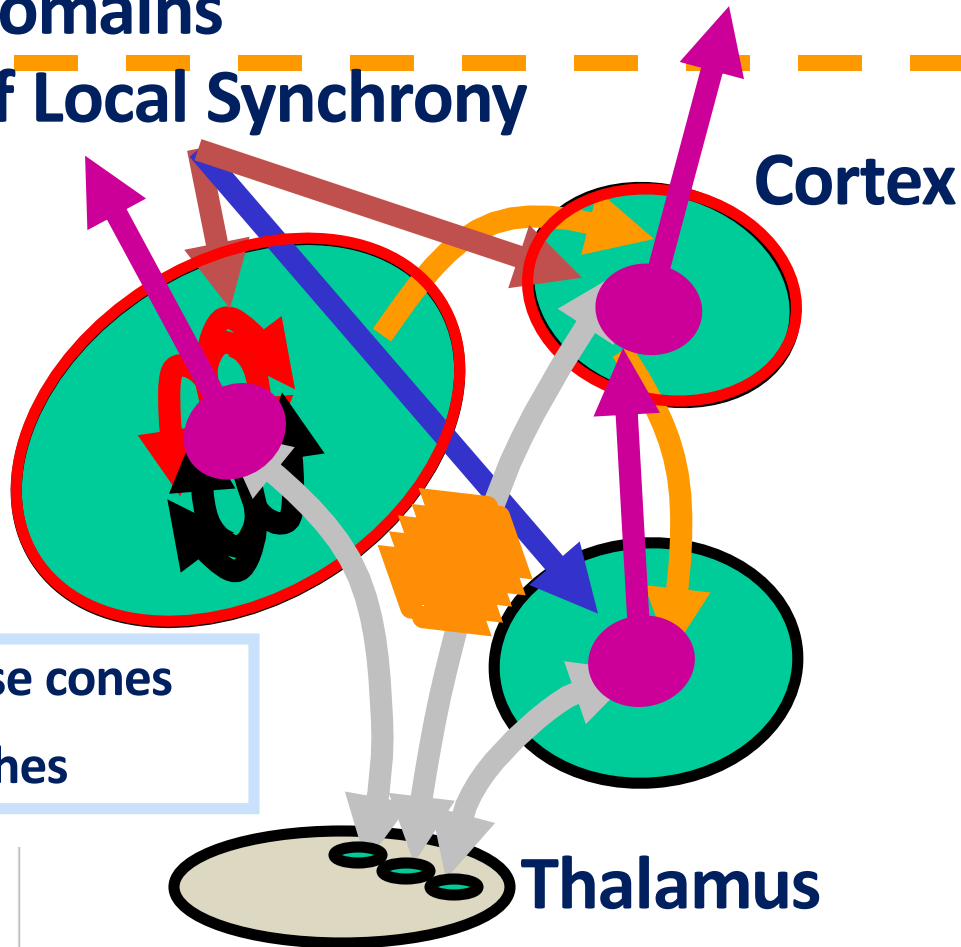
ICA Assumptions

- Mixing is linear at electrodes ✓
- Propagation delays are negligible ✓
- Component locations are fixed ?
- Component time courses are independent ?
- # components \leq # scalp channels ?



Are EEG effective source signals independent?

Independent
Domains
of Local Synchrony



Freeman - phase cones

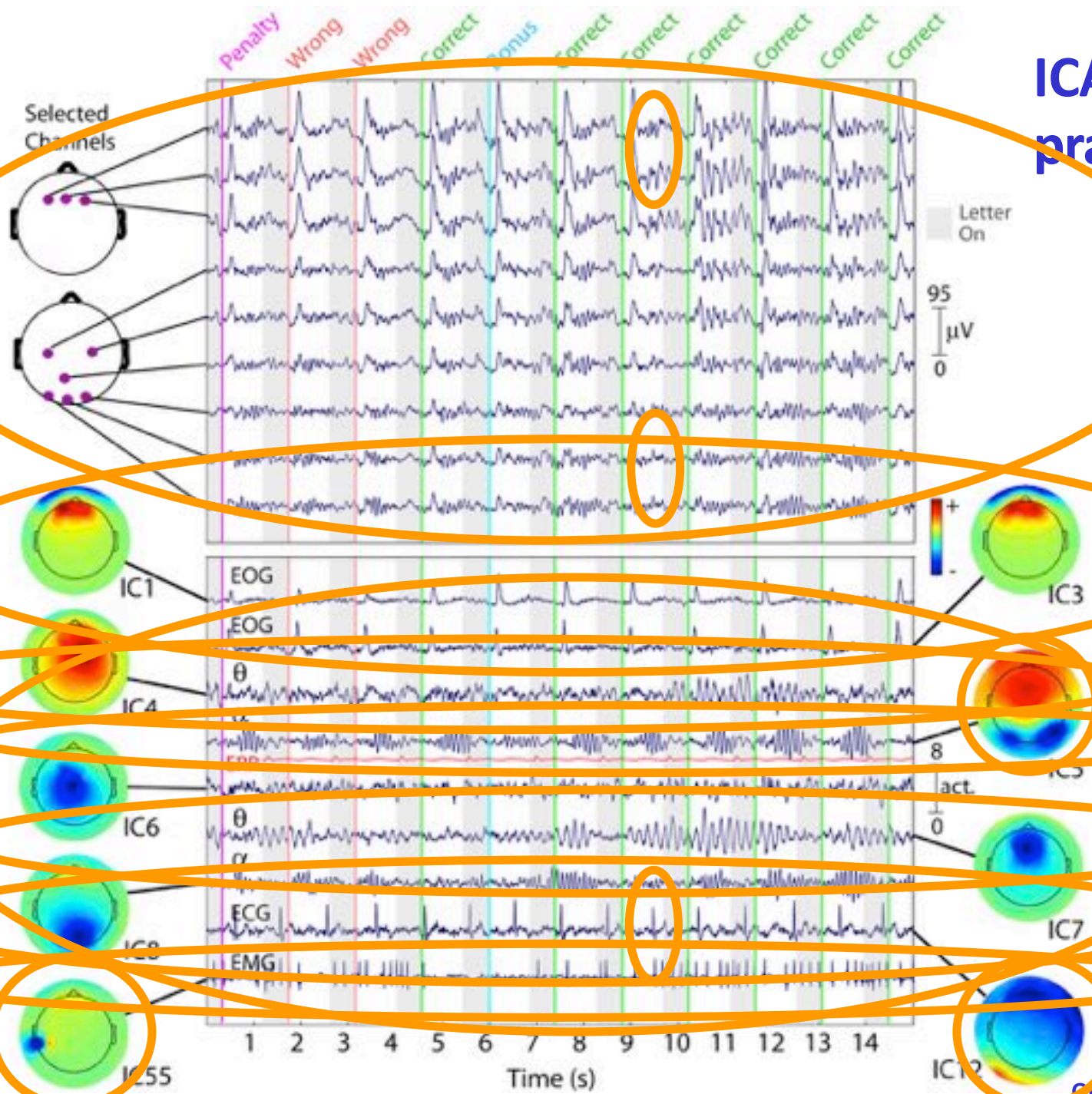
Plenz - avalanches

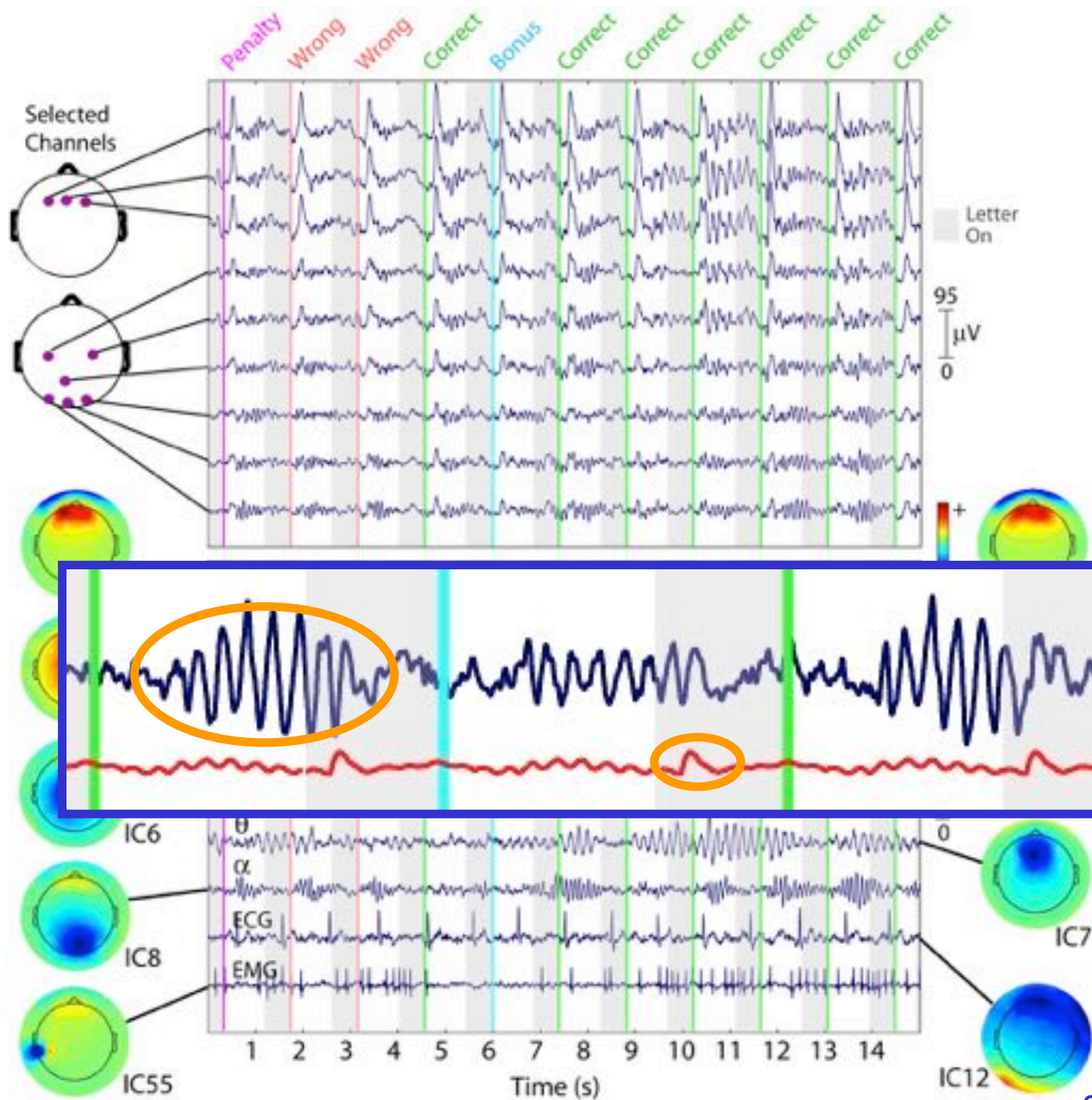
Properties of EEG Independent Components

- Maximally Temporally Independent
- Concurrently Active and Spatially Overlapping
- *Dipolar Scalp Maps* (Delorme et al., 2012)
- *Functionally Distinct*
- Between-Subject Similarity / Complexity

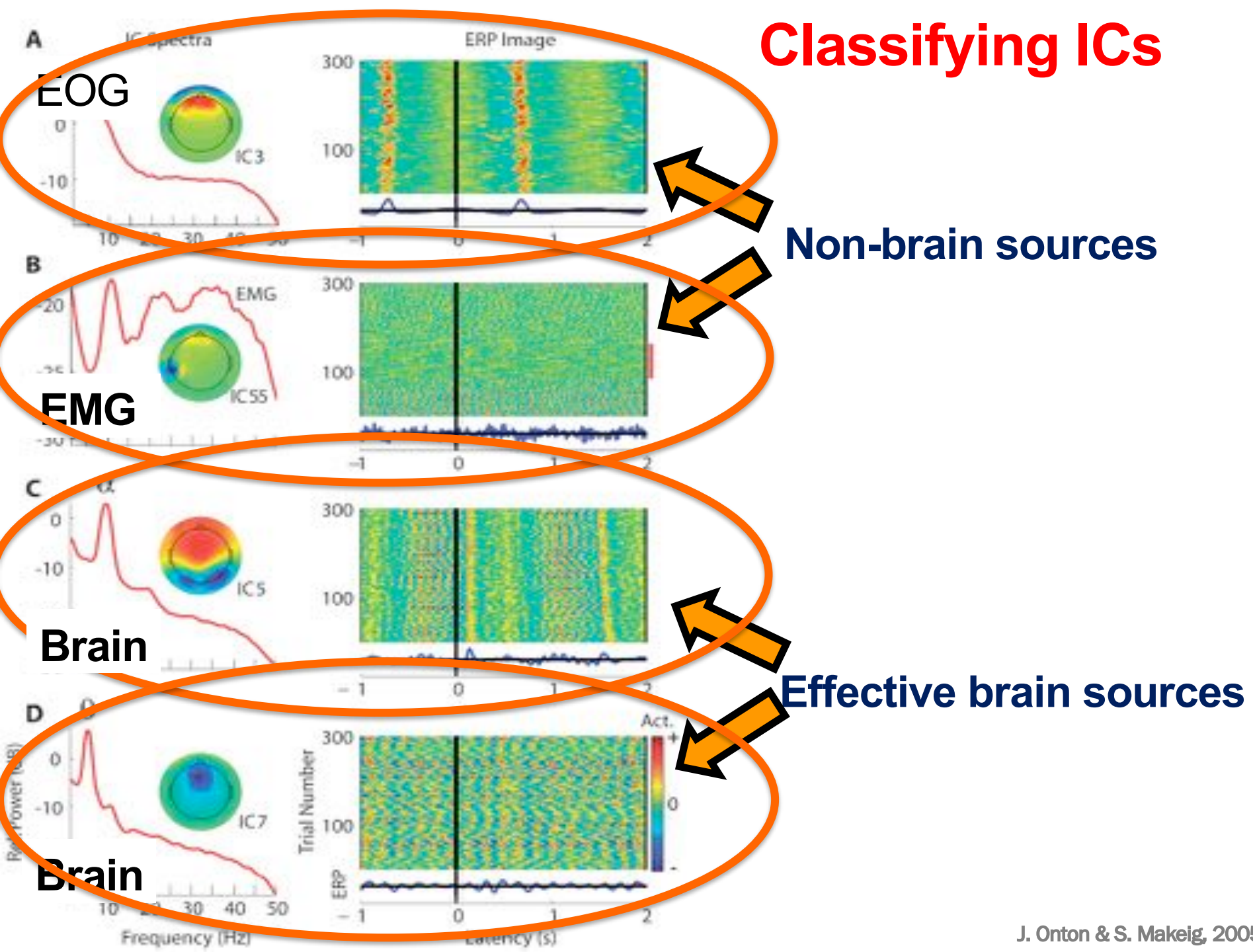


ICA in practice

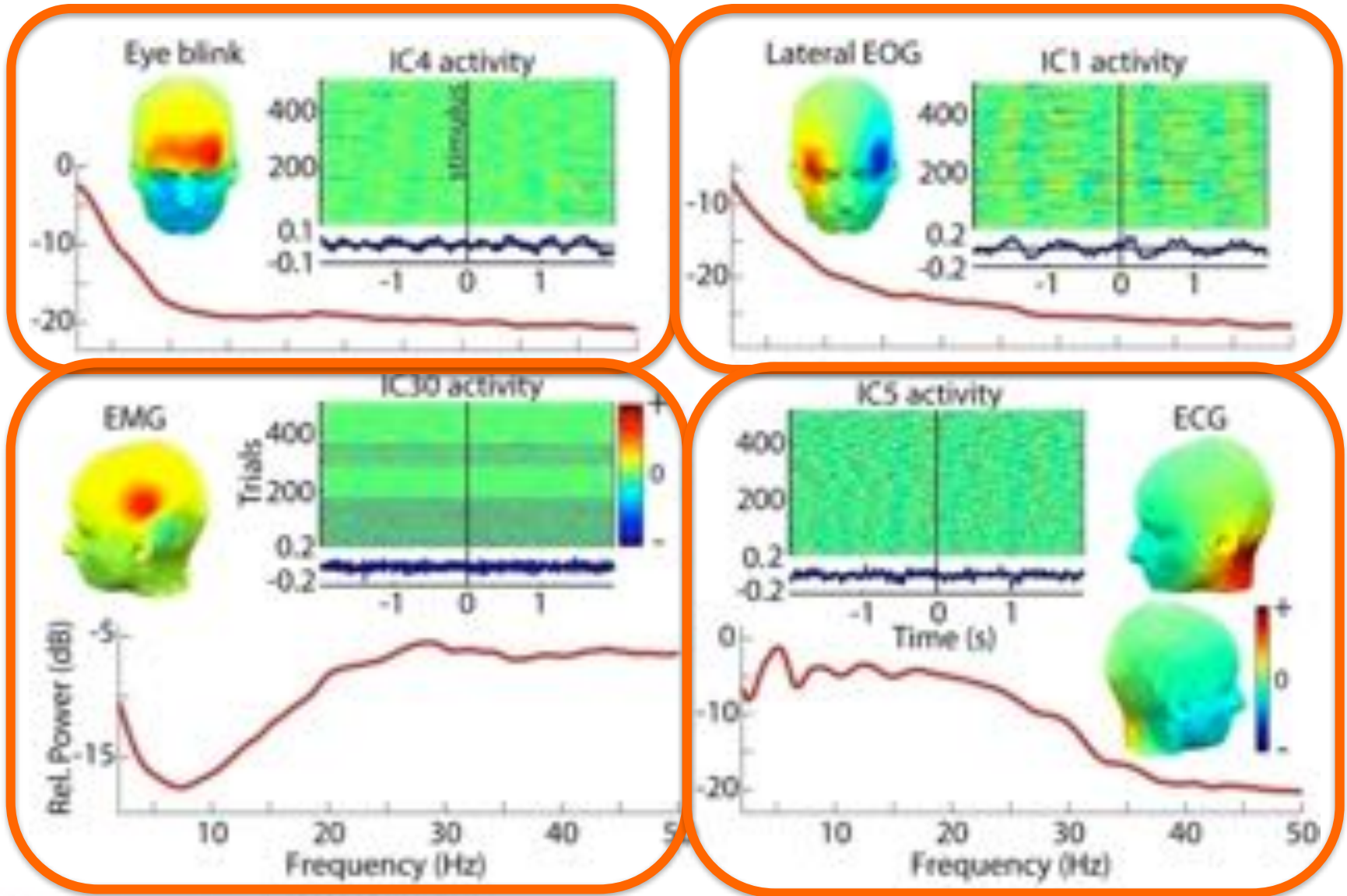




Classifying ICs

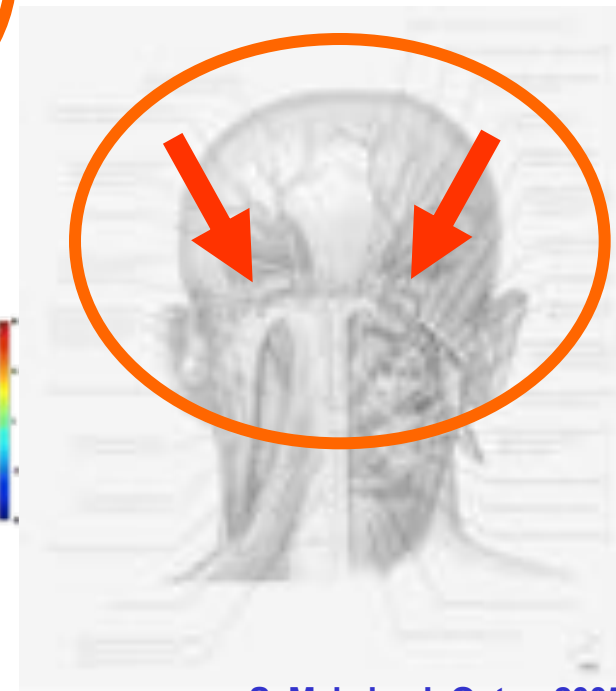
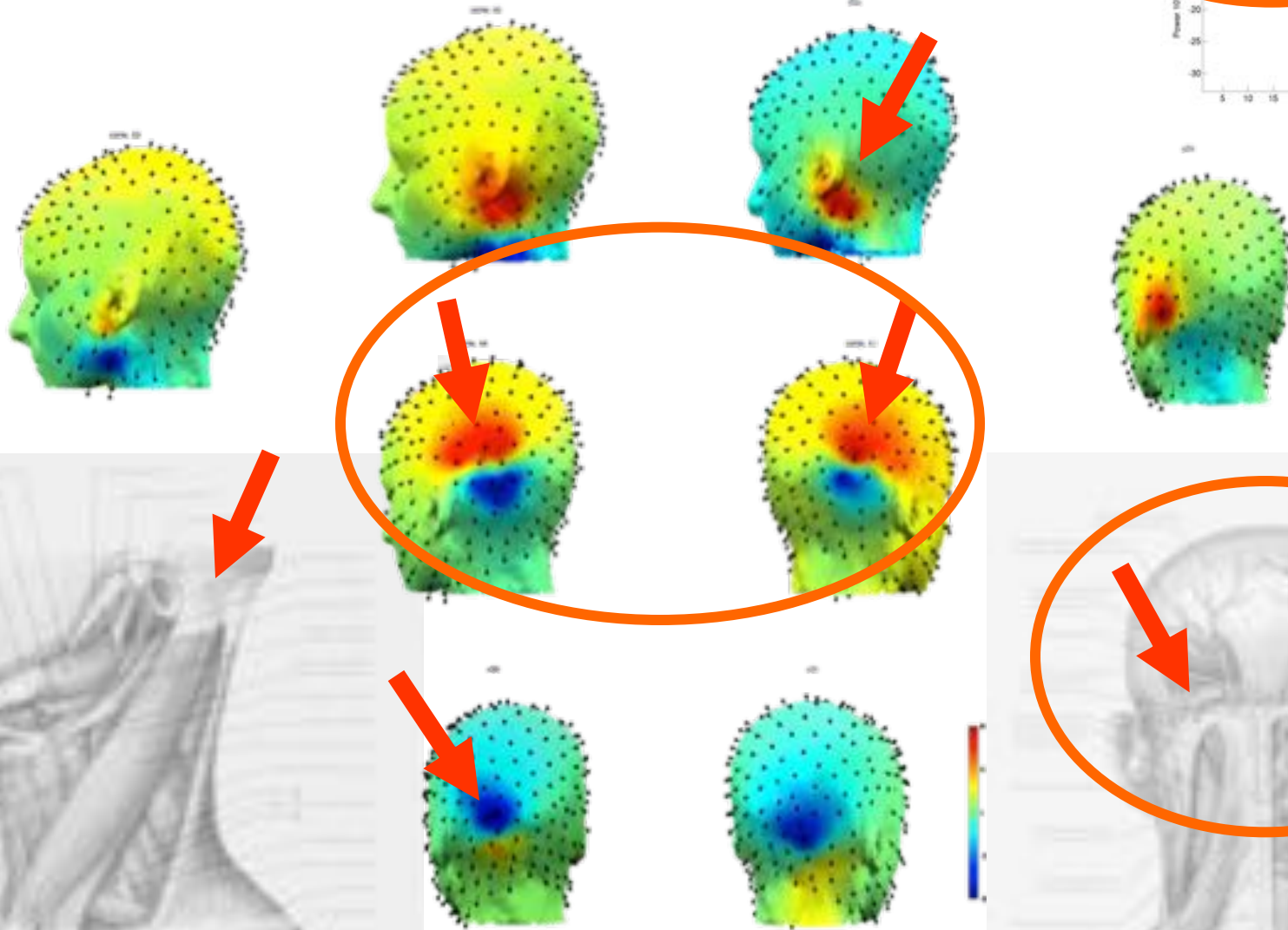
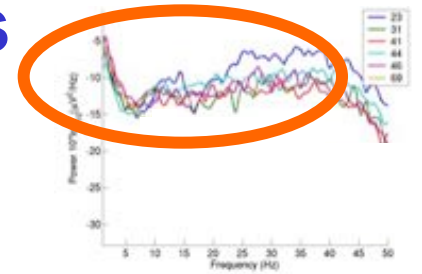


ICA finds Non-Brain Independent Component (IC) Processes ...

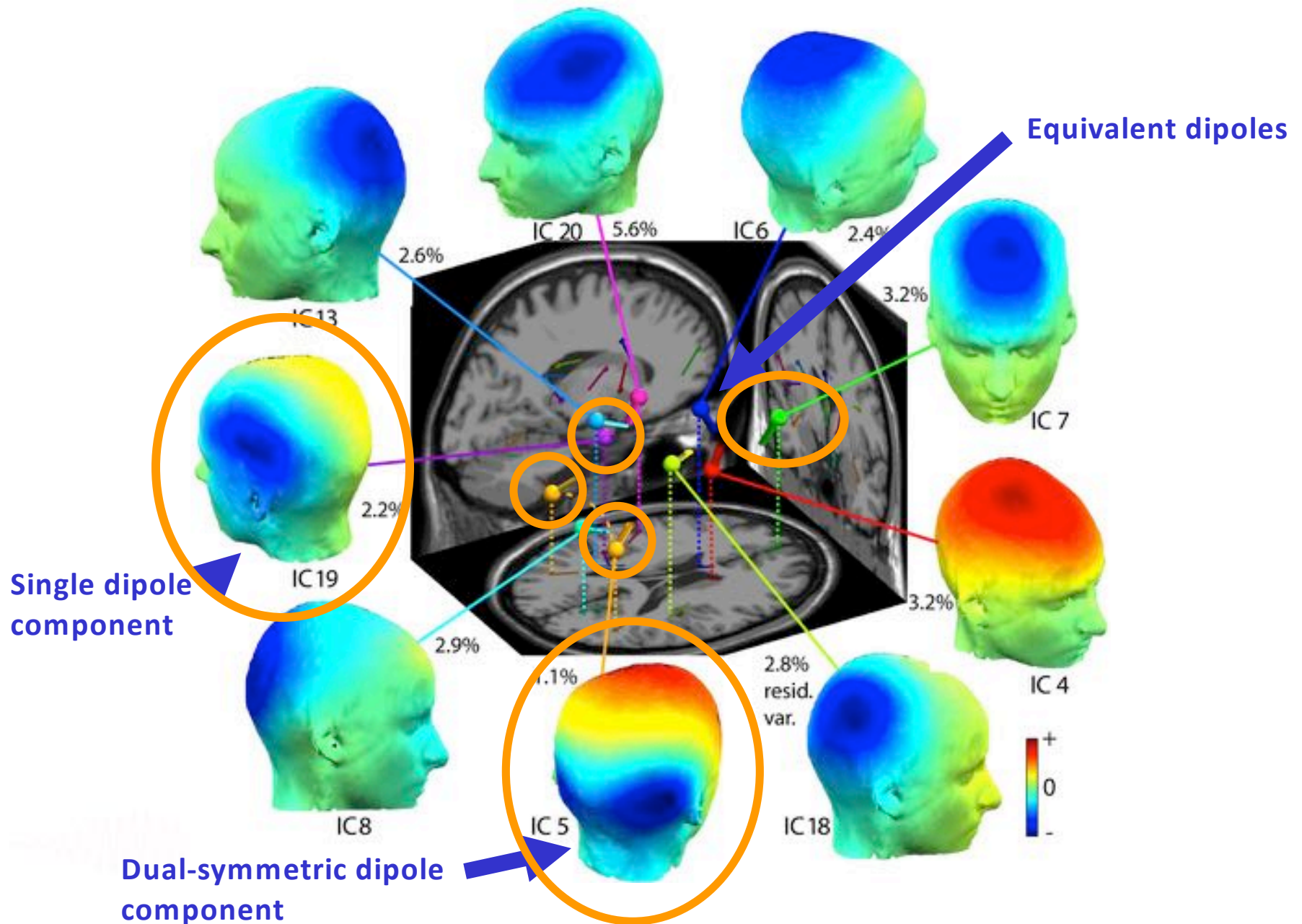


... separates them from the remainder of the data ...

Independent muscle signals



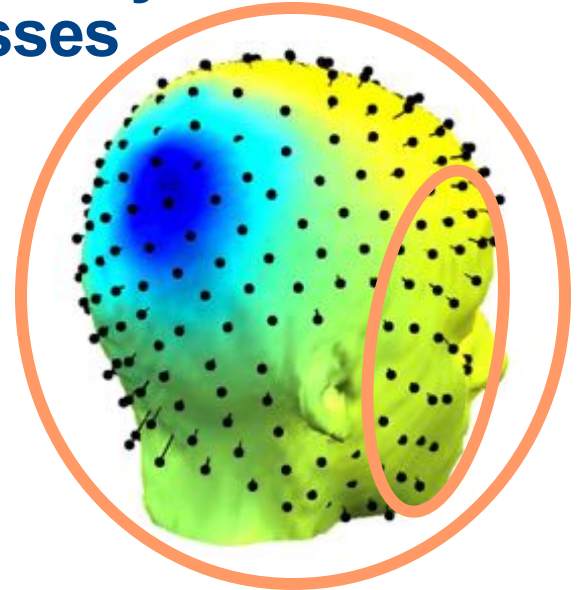
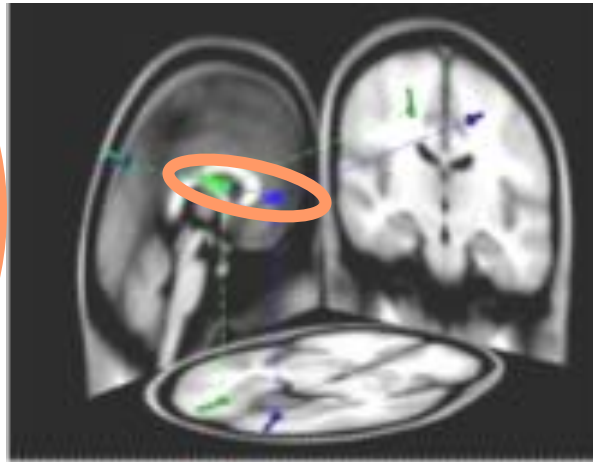
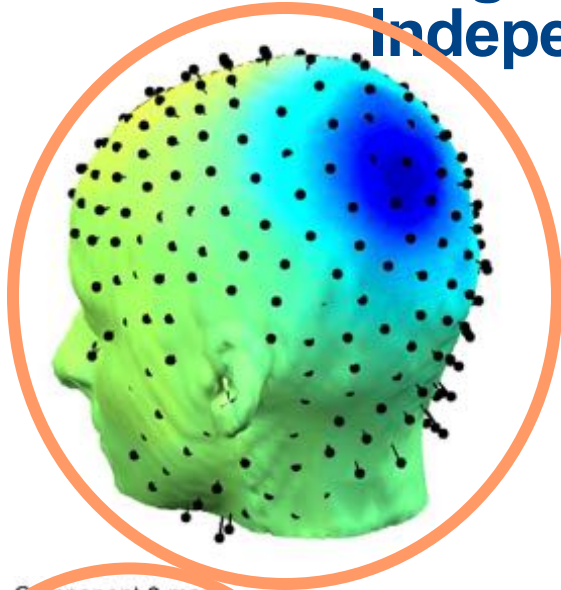
... and also separates cortical brain IC processes



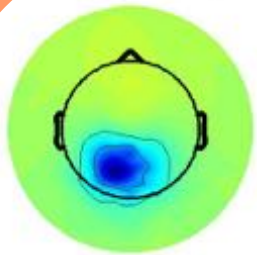
IC9

Single Session - Two Maximally Independent Alpha Processes

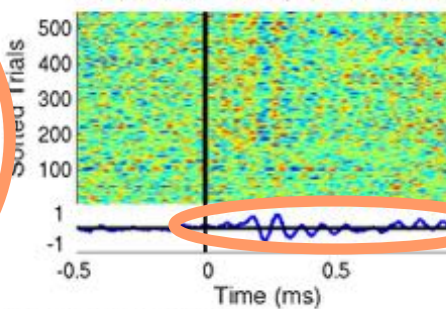
IC11



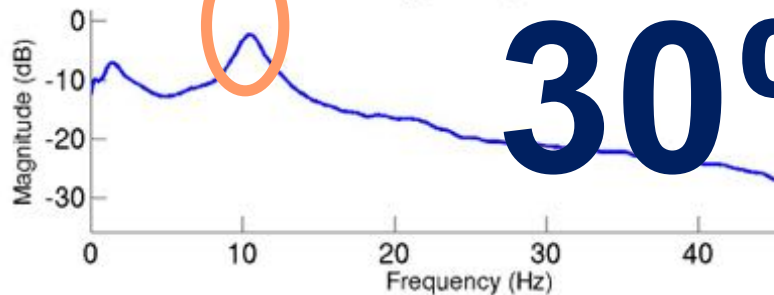
Component 9 map



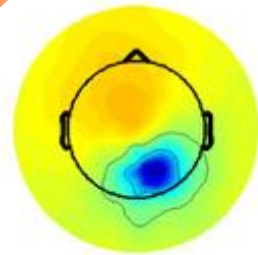
Component 9 activity (global offset 0.02)



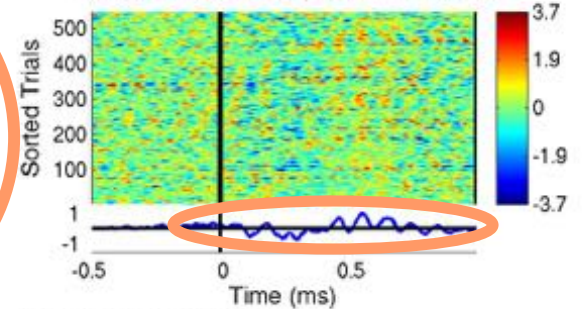
Activity power spectrum



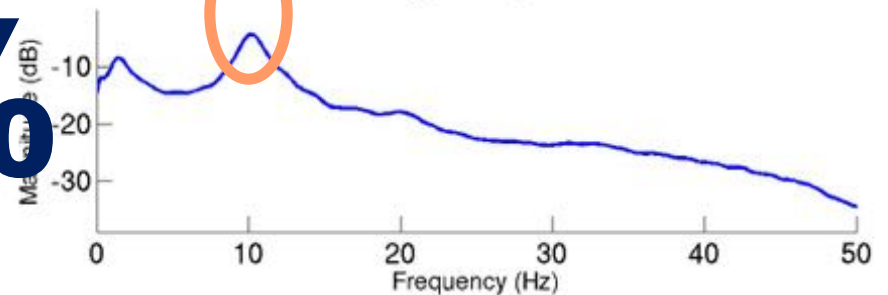
Component 11 map



Component 11 activity (global offset -0.038)



Activity power spectrum



30%

Important Result (2012)

Those **linear decompositions** of multi-channel EEG data that find ICs whose time courses are **more nearly** temporally **independent**

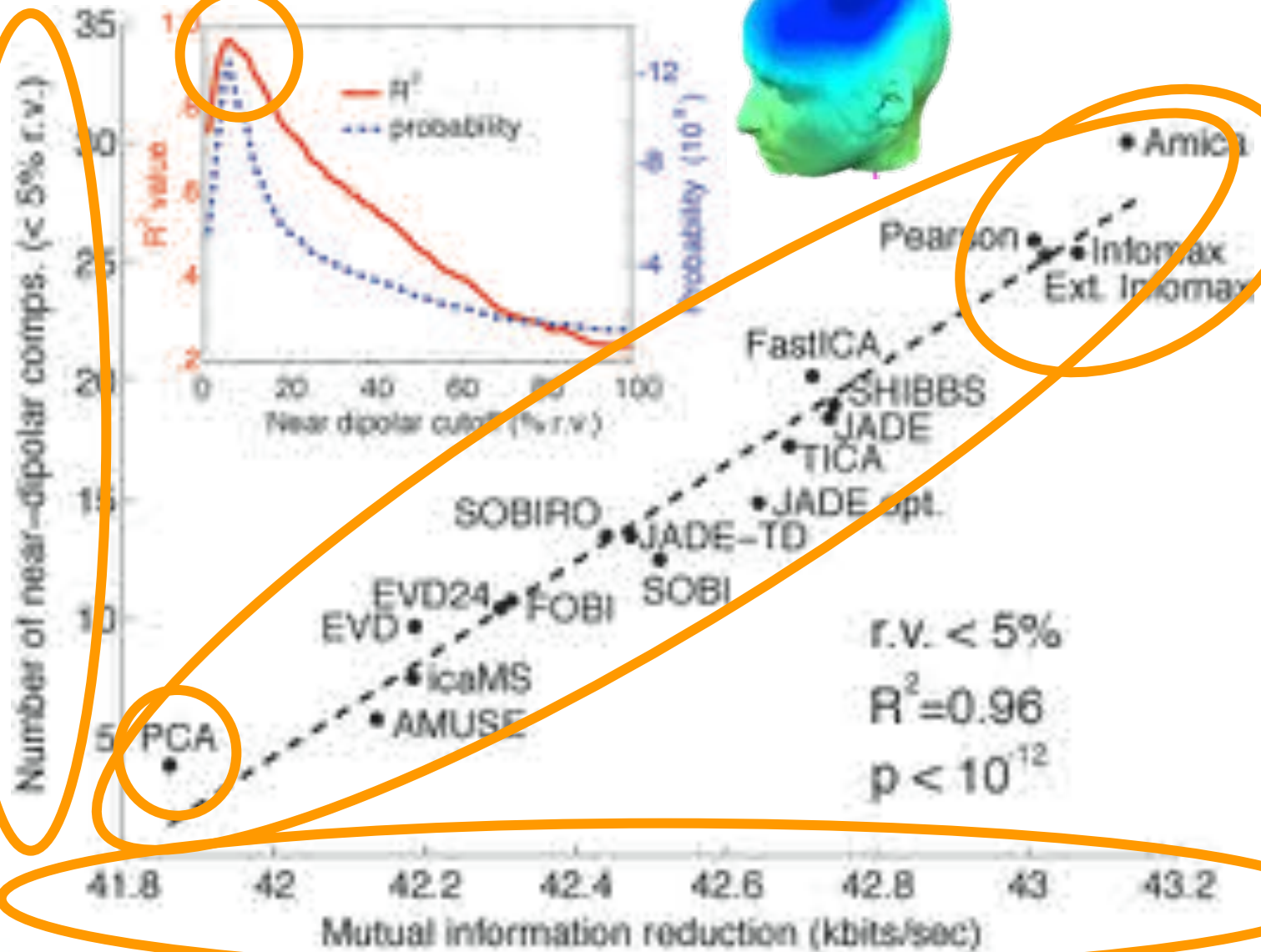
Also find more ICs whose scalp maps are highly '**dipolar**' – i.e., ICs compatible with the spatial projection of a source process in a single local cortical patch (or, a non-brain artifactual source)– *whose location can be accurately estimated* using a equivalent dipole model

More nearly *independent* component time courses



Larger number of *dipolar* component scalp projections

Hypothesis: Dipolar ICs = Localized effective source processes



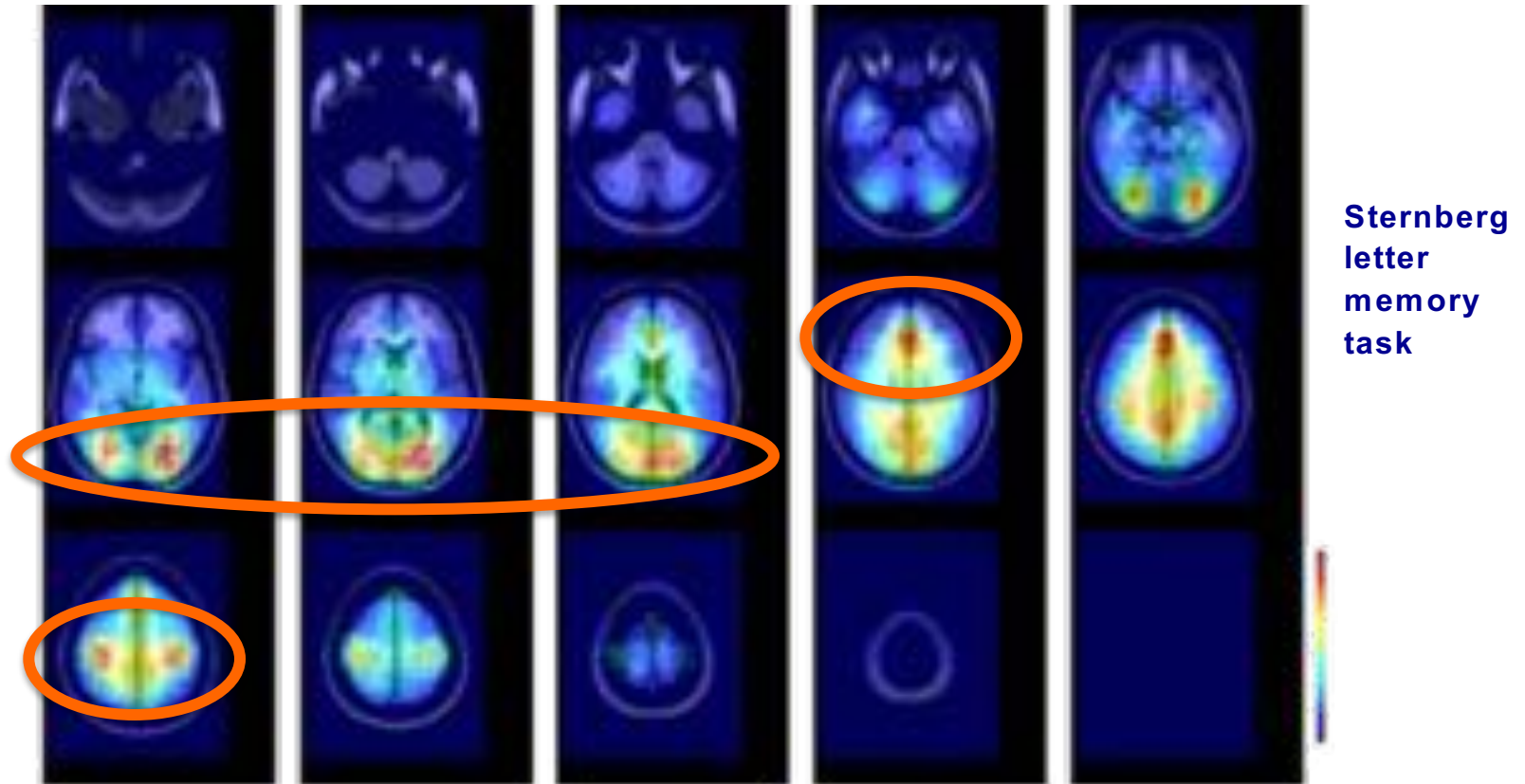
The background features a central brain diagram with various colored regions and lines. Surrounding this are several 3D head models, each with a different colored map representing brain activity. Labels for these models include IC 13, IC 20 (1.5%), IC 6, IC 7, IC 19, IC 8, IC 5, IC 18, and IC 4. A color scale on the right ranges from -1 to 1. Percentages for some models are: IC 13 (24%), IC 20 (1.5%), IC 6 (24%), IC 19 (23%), IC 8 (24%), IC 5 (1.1%), IC 18 (2.0% resid. var.), and IC 4 (2.0%).

Are locations of EEG *effective sources* similar across tasks?

Are *effective source* locations within task similar across participants?

Effective Source Density

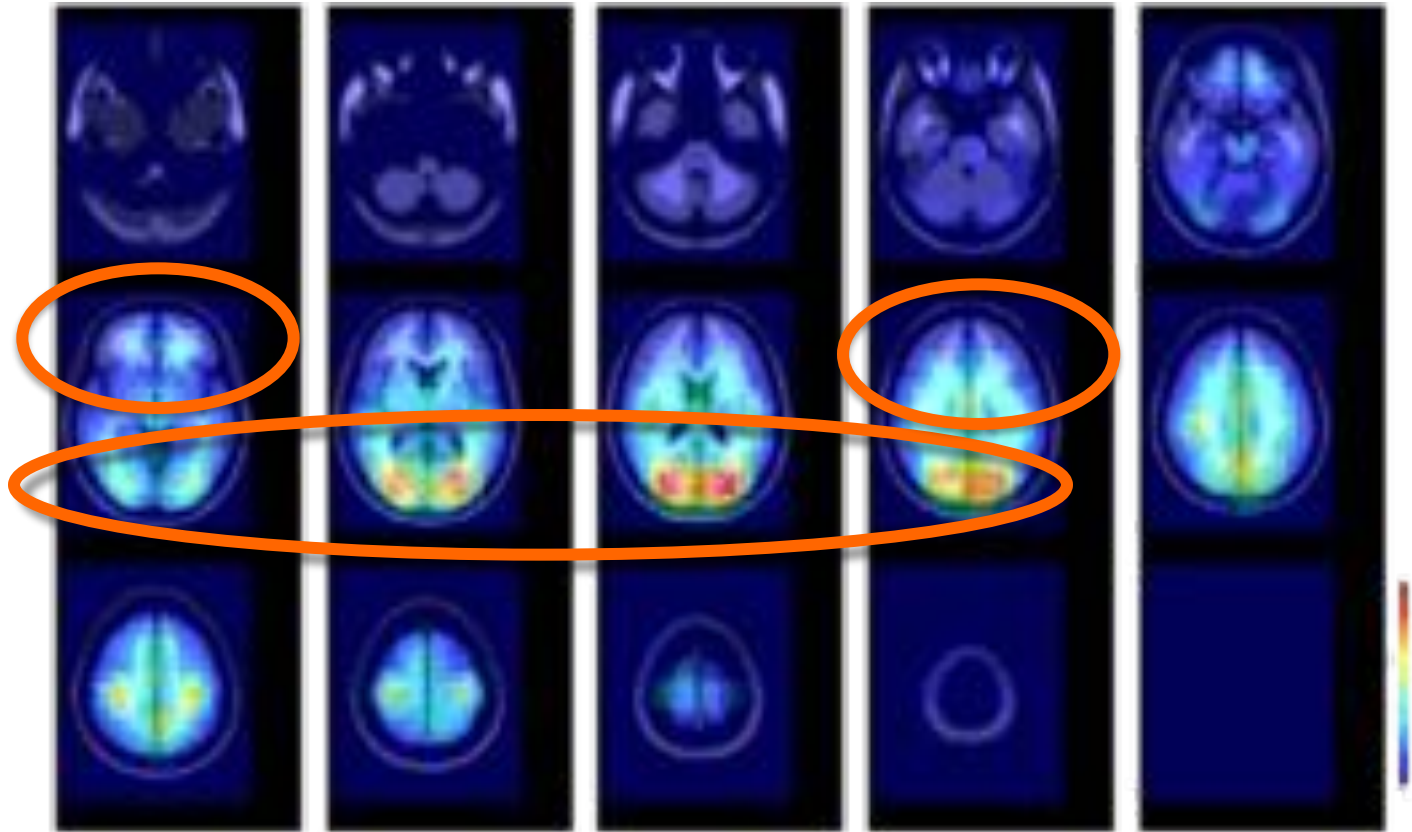
Visual Working Memory



dipoledensity()

Effective Source Density

Eyes-closed emotion imagination

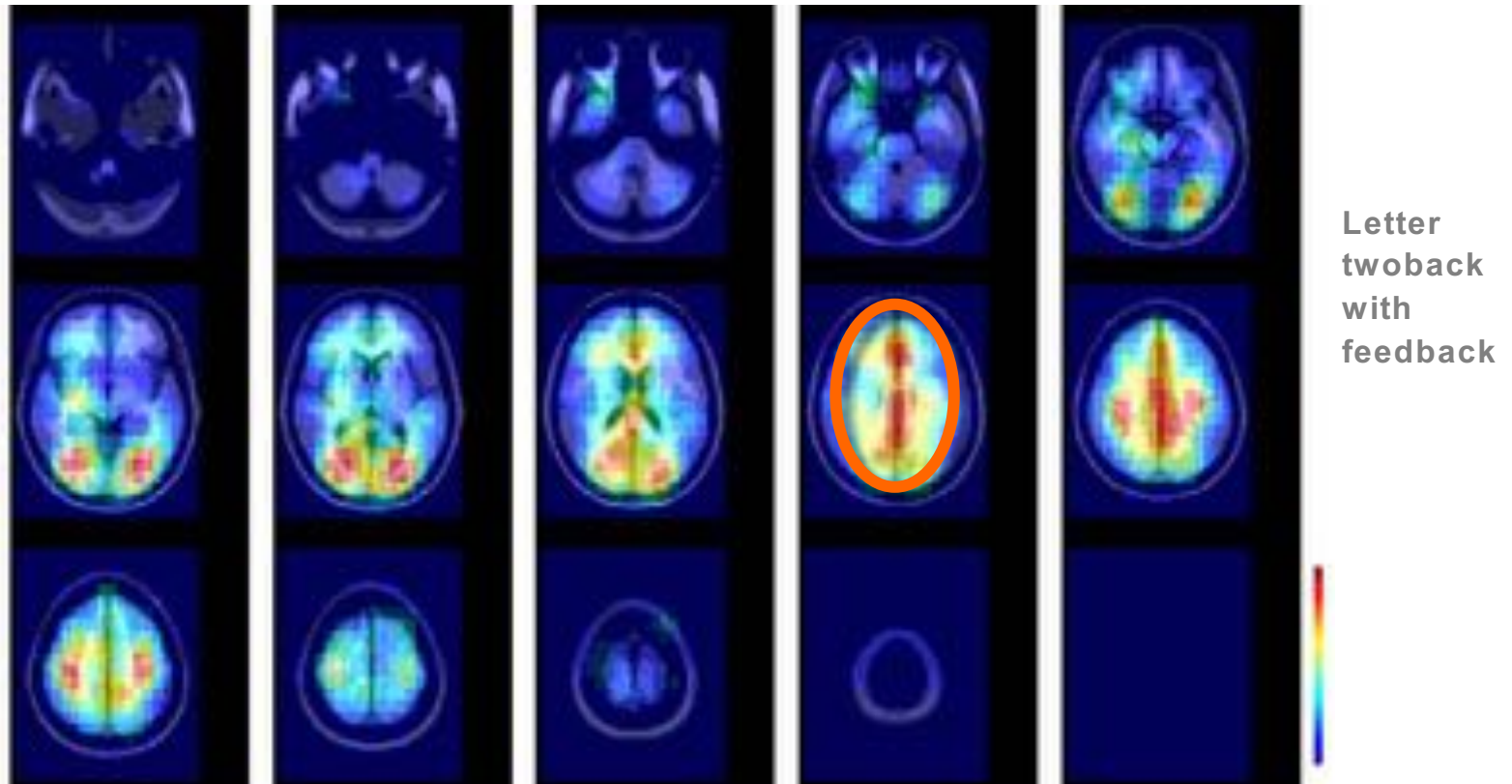


>> dipoledensity()



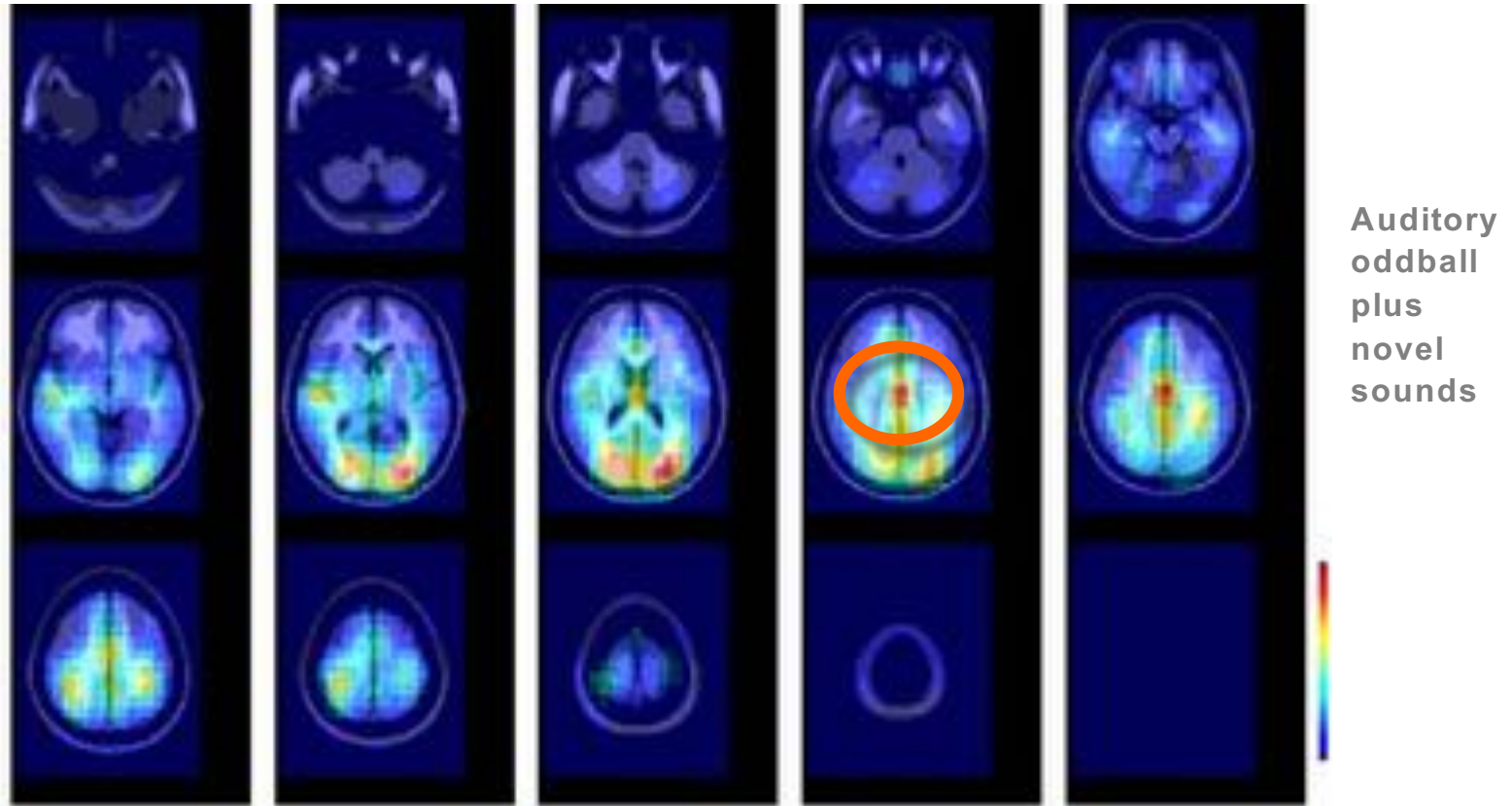
Effective Source Density

Letter twoback with feedback



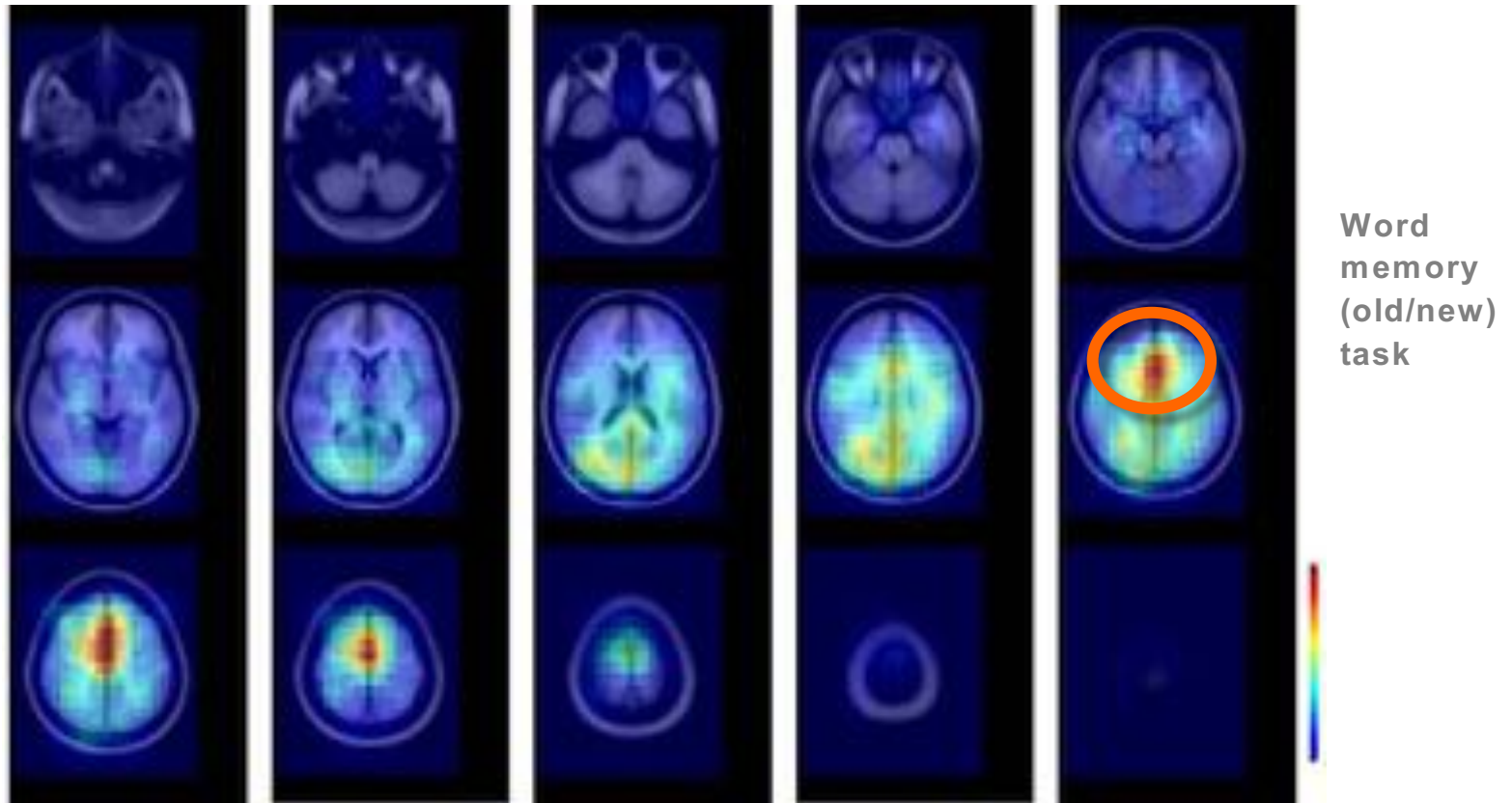
Effective Source Density

Auditory novelty oddball



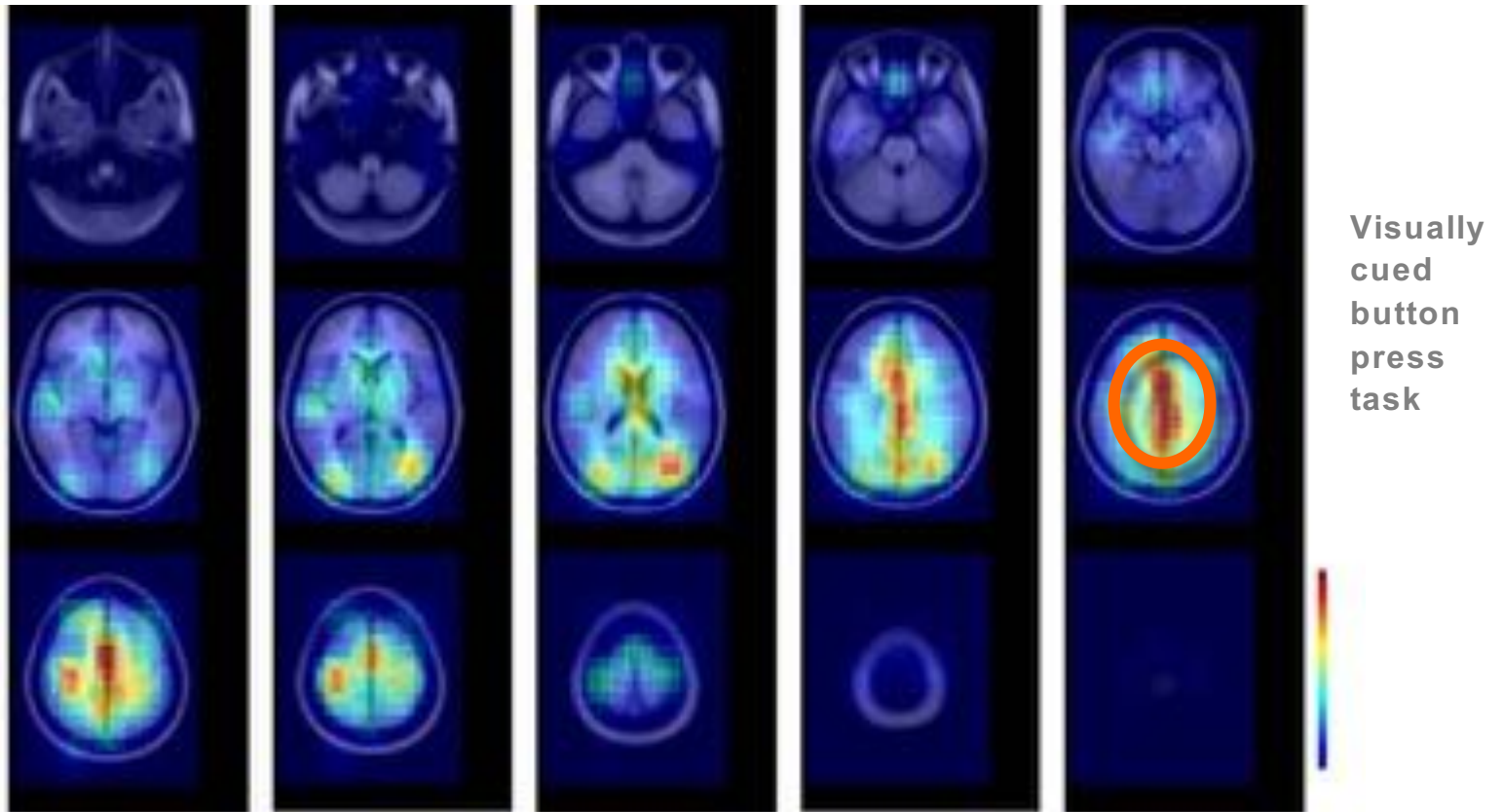
Effective Source Density

A. Old/new word memory



Effective Source Density

B. Visually cued selective response



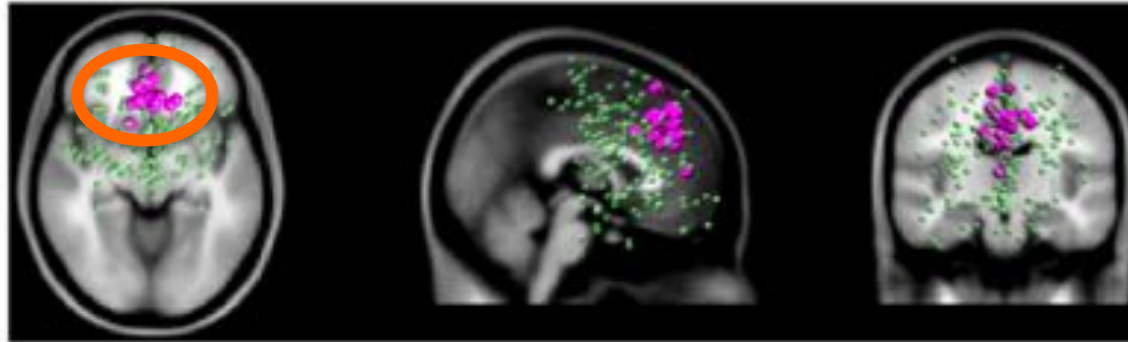
Are source dynamics similar across participants?



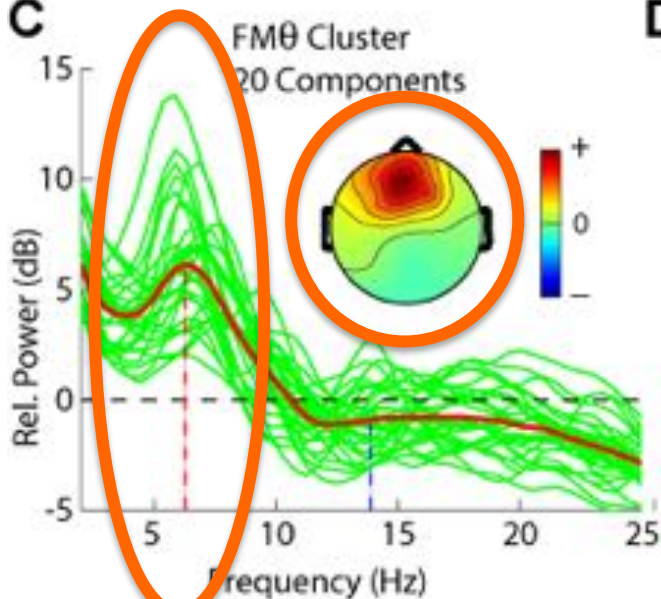
Example: frontal midline theta cluster

B

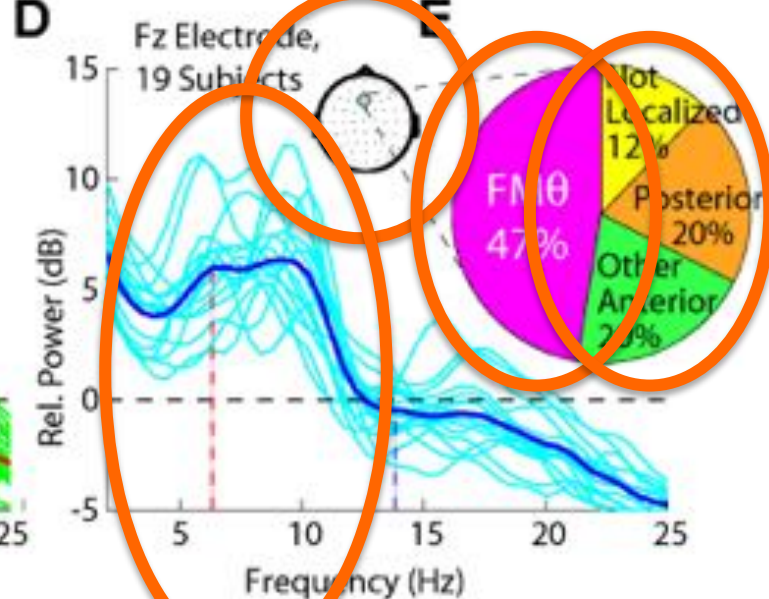
FM θ Cluster



C

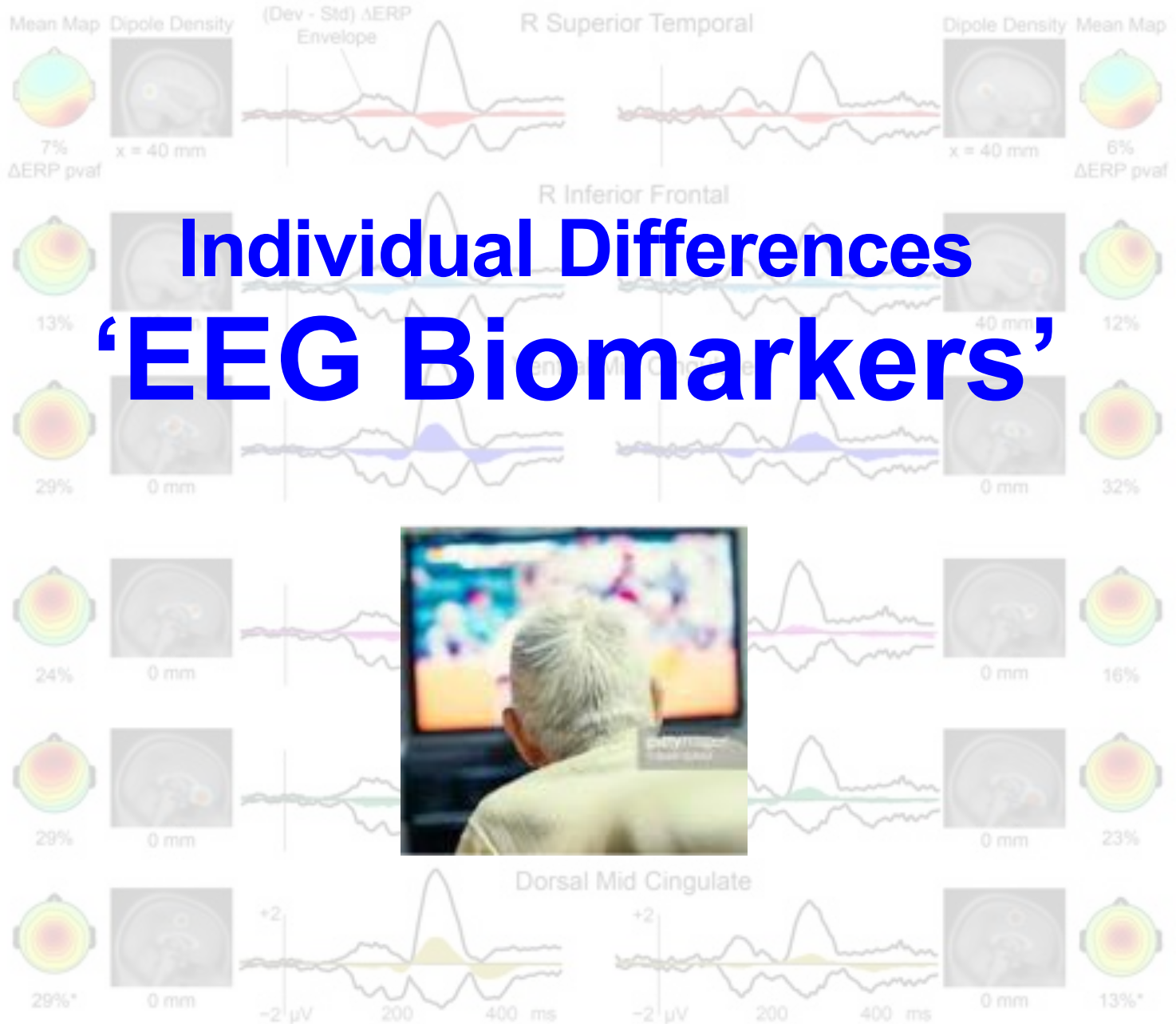


D



Nonpsychiatric Comparison Subjects (NCS)

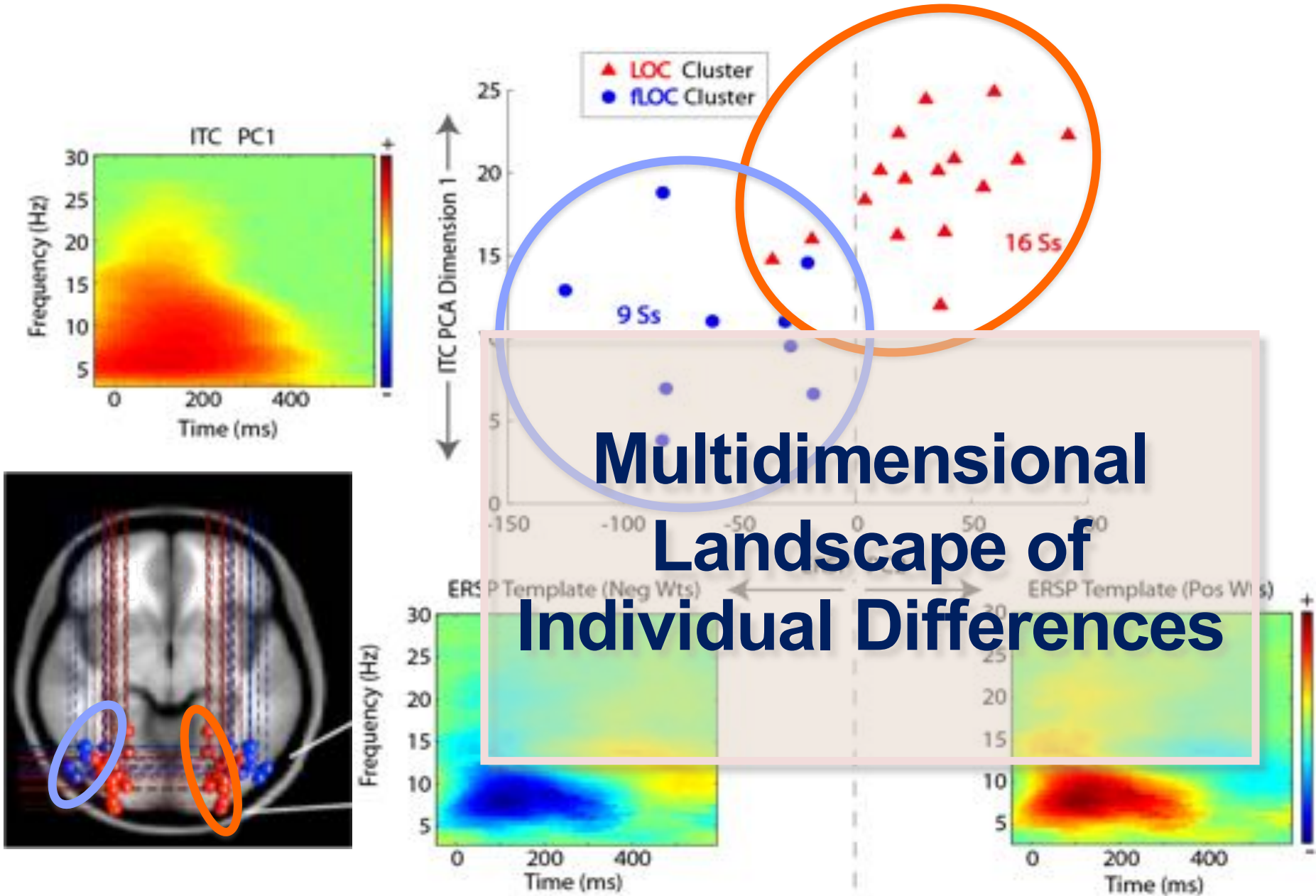
Schizophrenia Patients (SZ)

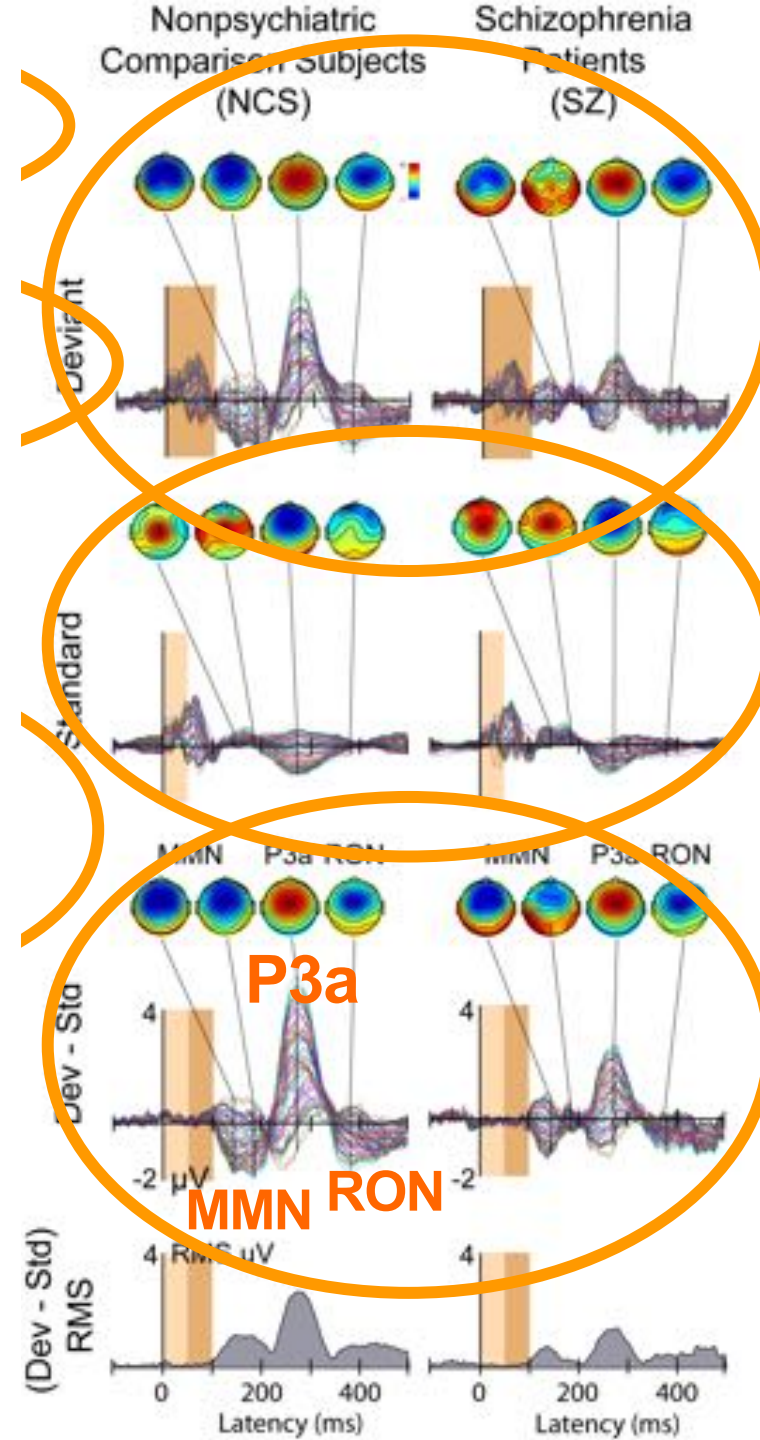


Individual Differences 'EEG Biomarkers'

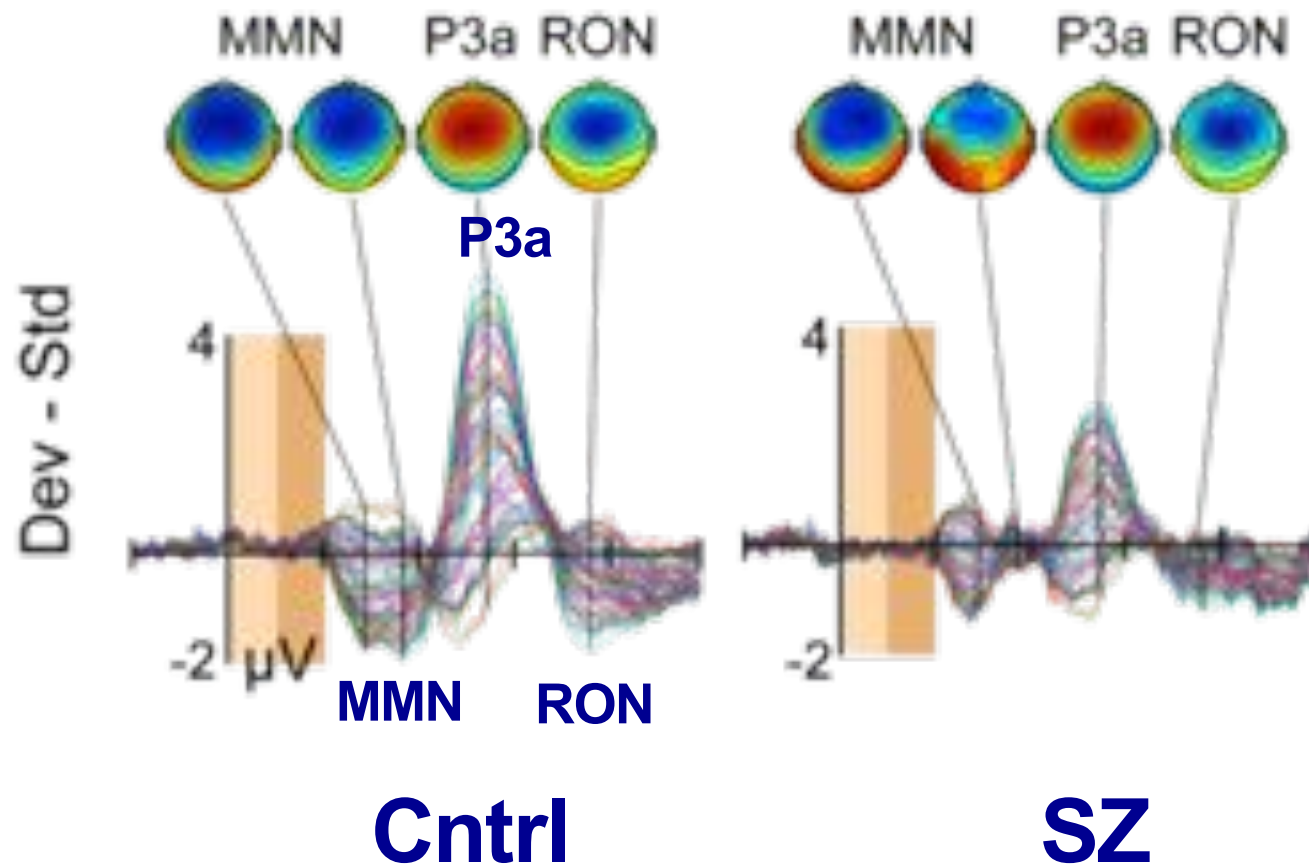


Can ICA reveal subject differences?





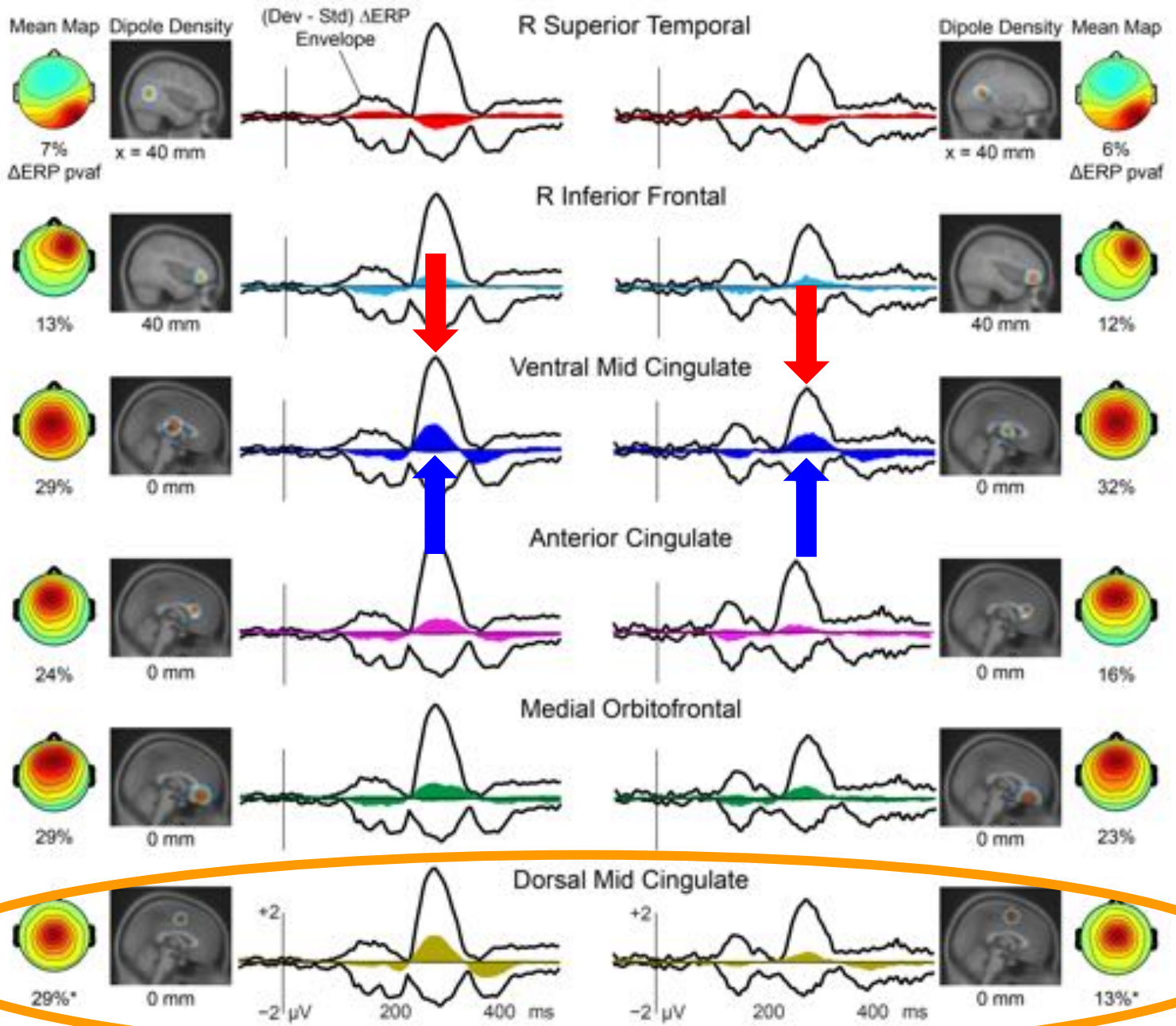
Auditory Deviance Response



The deepest mental trap in electrophysiology
lurks in the word "THE" !!!

Nonpsychiatric Comparison Subjects (NCS)

Schizophrenia Patients (SZ)



PEAK AMPLITUDES

ERP

r²

Scalp Electrode (Fz)

Verbal IQ (WRAT)	P3a	0.11
Functional Capacity (UPSA)	RON	0.12

X

R Superior Temporal

Working Memory (LNS Reorder)	RON	0.15
Verbal IQ (WRAT)	RON	0.15
Immediate Verbal Memory (CVLT)	RON	0.28
Delayed Verbal Memory (CVLT)	RON	0.26
Functional Capacity (UPSA)	MMN	0.48
Functional Capacity (UPSA)	RON	0.26

R Inferior Frontal

Negative Symptoms (SANS)	RON	0.36
Psychosocial Functioning (SOF)	RON	0.24
Auditory Attention (LNS Forward)	MMN	0.38
Working Memory (LNS Reorder)	MMN	0.30
Verbal IQ (WRAT)	MMN	0.46

Ventral Mid Cingulate

Positive Symptoms (SAPS)	RON	0.29
Negative Symptoms (SANS)	P3a	0.36
Immediate Verbal Memory (CVLT)	RON	0.41
Delayed Verbal Memory (CVLT)	RON	0.24
Verbal IQ (WRAT)	RON	0.29
Executive Functioning (WCST)	RON	0.24

Anterior Cingulate

Functional Status (GAF)	MMN	0.18
Functional Status (GAF)	RON	0.17
Immediate Verbal Memory (CVLT)	RON	0.25
Delayed Verbal Memory (CVLT)	RON	0.17

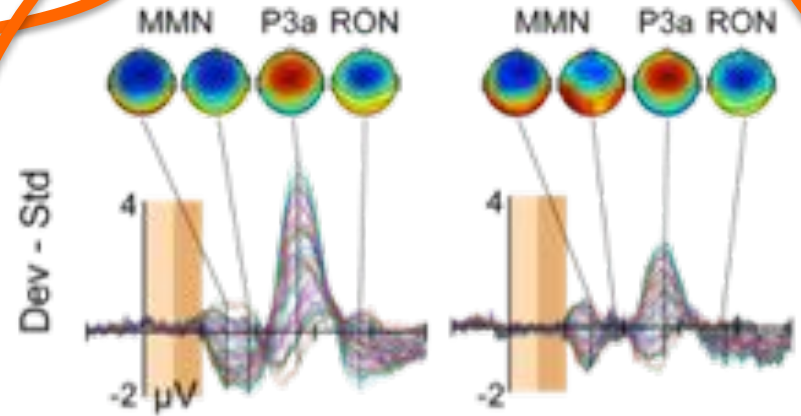
Medial Orbitofrontal

Positive Symptoms (SAPS)	P3a	0.40
Negative Symptoms (SANS)	P3a	0.54
Psychosocial Functioning (SOF)	P3a	0.37
Functional Capacity (UPSA)	P3a	0.32

Dorsal Mid Cingulate

Verbal IQ (WRAT)	P3a	0.15
Executive Functioning (WCST)	MMN	0.18

ADR



Cntrl

SZ

PEAK LATENCIES

ERP

r²

Scalp Electrode (Fz)

---n/a---

R Superior Temporal

Functional capacity (UPSA)

MMN

0.25

Delayed Verbal Memory (CVLT)

MMN

0.17

R Inferior Frontal

Negative Symptoms (SANS)

RON

0.51

Psychosocial Functioning (SOF)

RON

0.25

Executive Functioning (WCST)

MMN

0.30

Executive Functioning (WCST)

P3a

0.28

Ventral Mid Cingulate

Negative Symptoms (SANS)

P3a

0.33

Negative Symptoms (SANS)

RON

0.33

Psychosocial Functioning (SOF)

P3a

0.31

Verbal IQ (WRAT)

MMN

0.25

Executive Functioning (WCST)

P3a

0.30

Anterior Cingulate

Functional Capacity (UPSA)

RON

0.17

Verbal IQ (WRAT)

MMN

0.24

Auditory Attention (LNS-Forward)

MMN

0.17

Medial Orbitofrontal

Negative Symptoms (SANS)

RON

0.41

Positive Symptoms (SAPS)

RON

0.40

Auditory Attention (LNS-Forward)

MMN

0.29

Executive Functioning (WCST)

P3a

0.32

Dorsal Mid Cingulate

Negative Symptoms (SANS)

MMN

0.20

Negative Symptoms (SANS)

P3a

0.17

Global Functioning (GAF)

RON

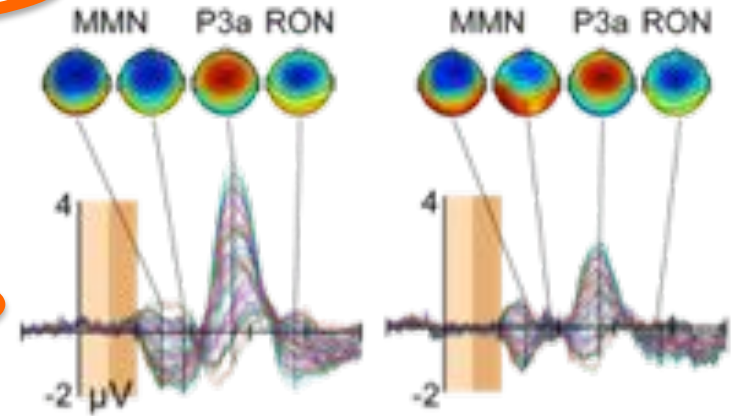
0.24

Functional Capacity (UPSA)

P3a

0.13

ADR



Cntrl

SZ

Nonpsychiatric Comparison Subjects (NCS)

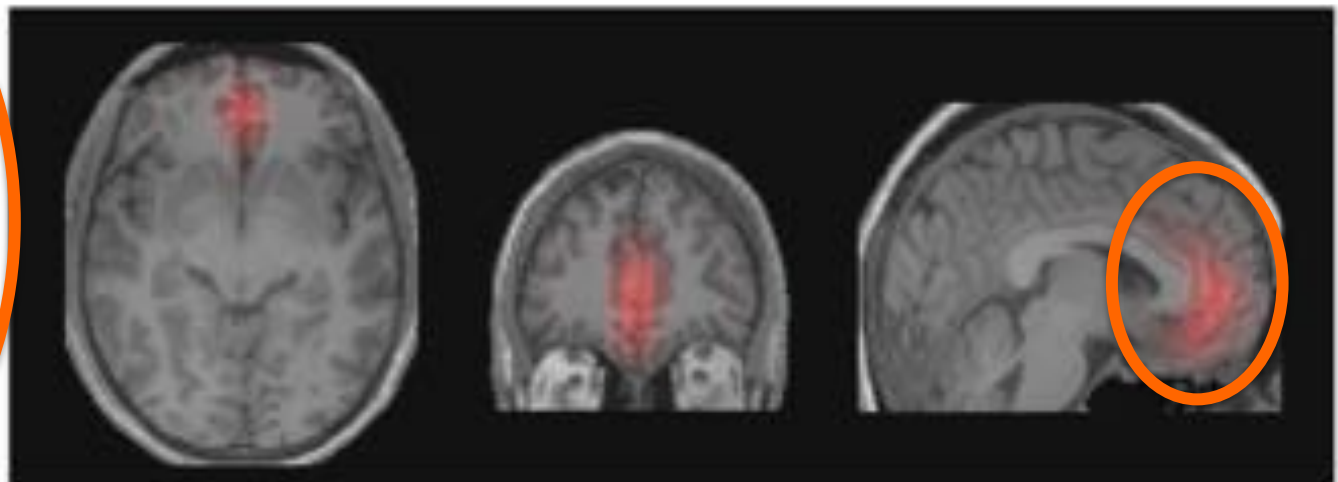
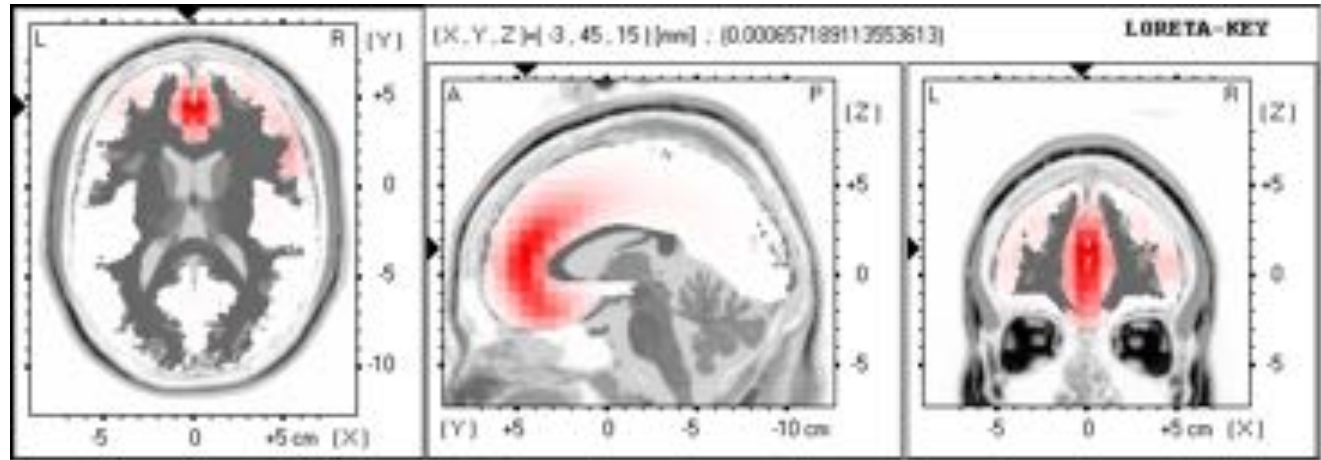
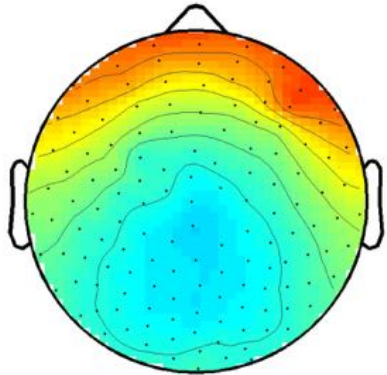
Schizophrenia Patients (SZ)

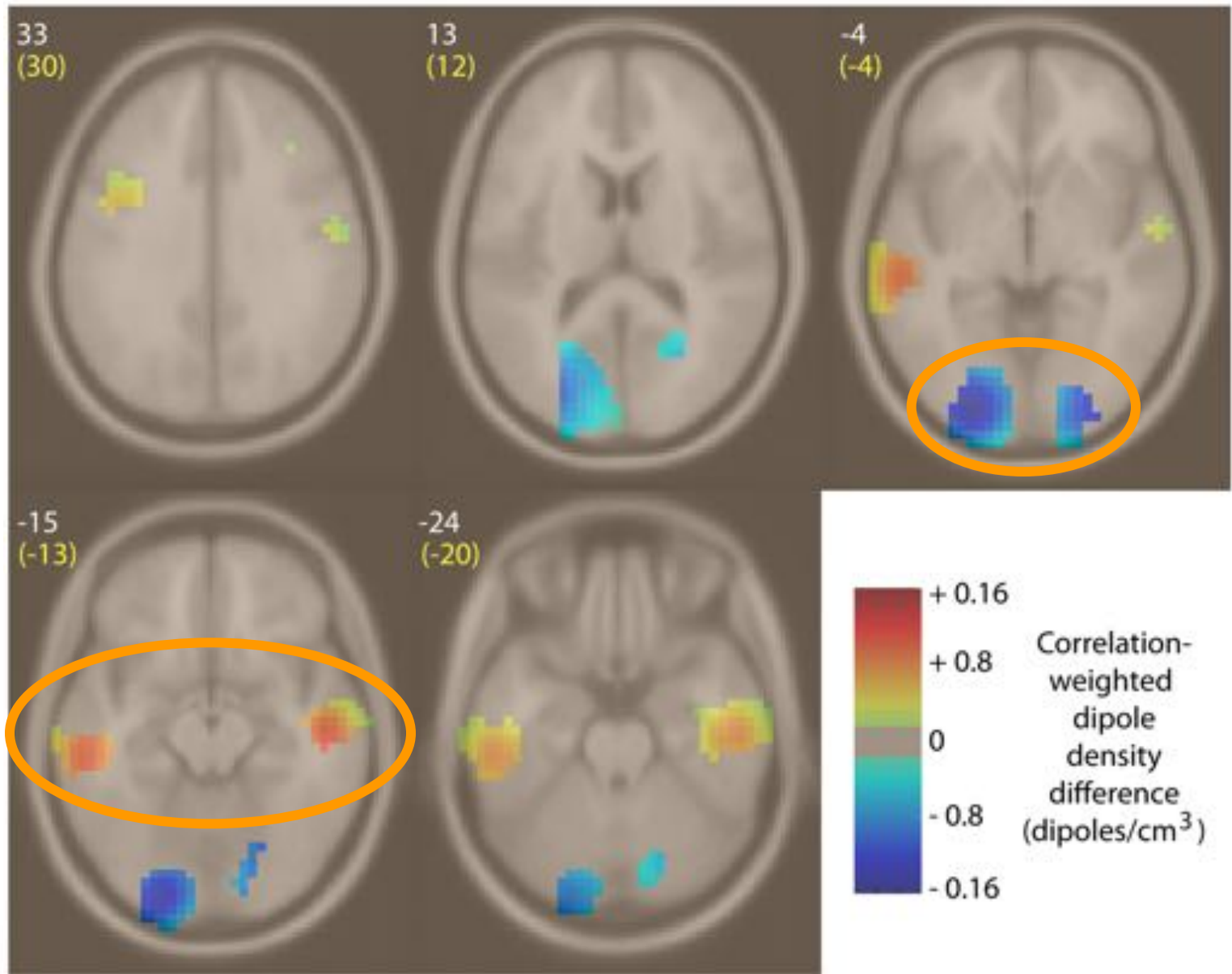


Low- and High-Resolution Source Localization

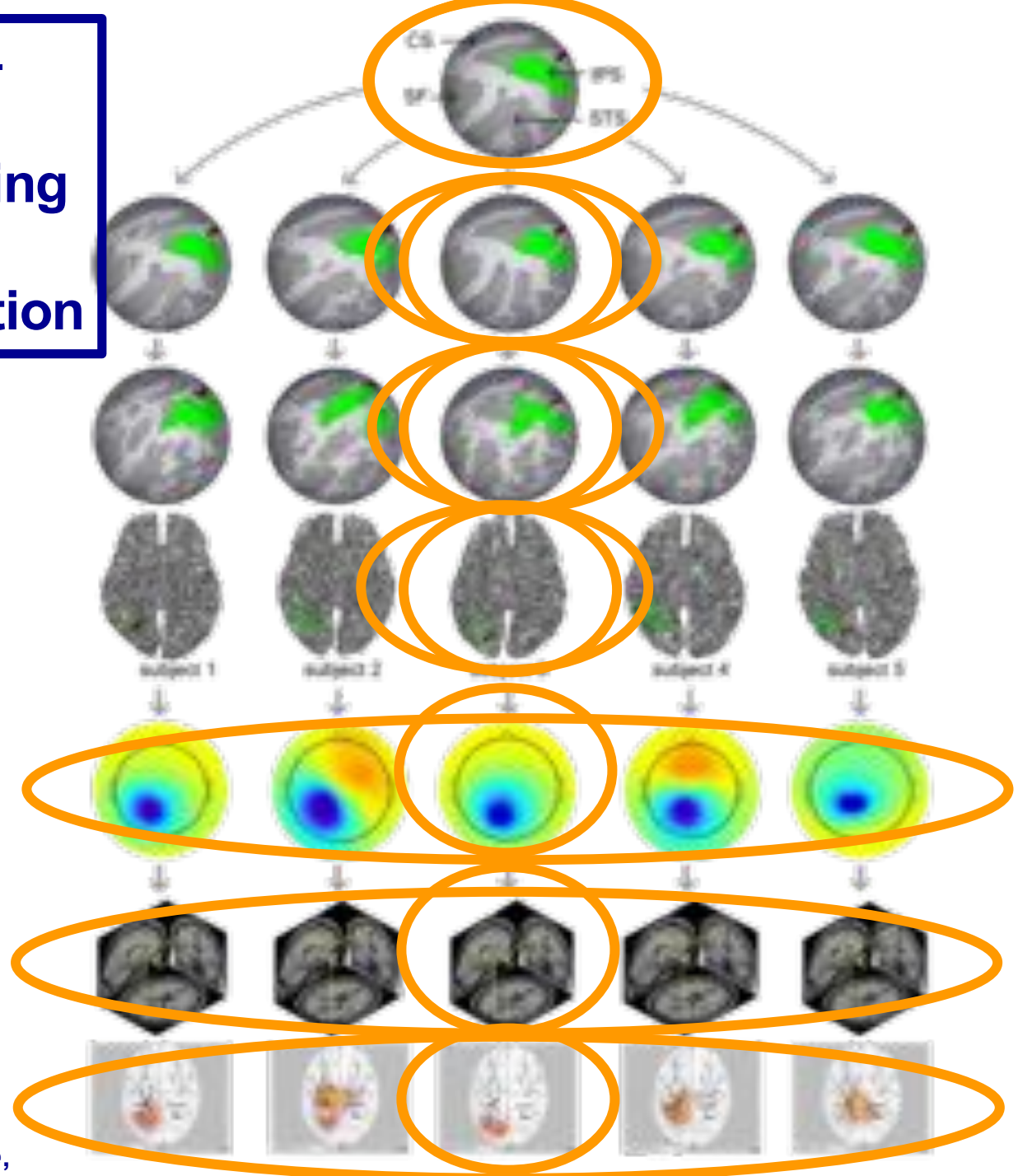
EEG Source Localization

LORETA = **Low-Resolution** Electrical Tomography





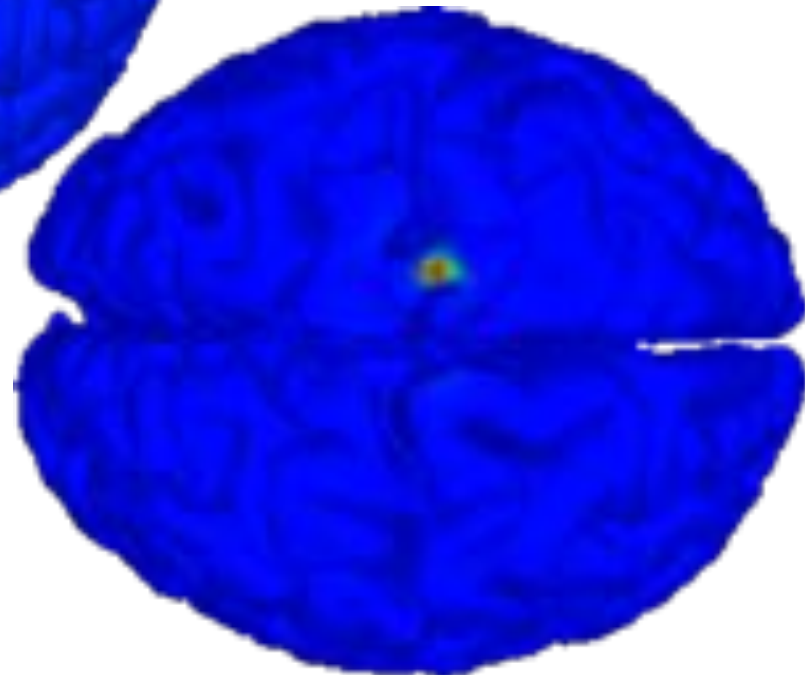
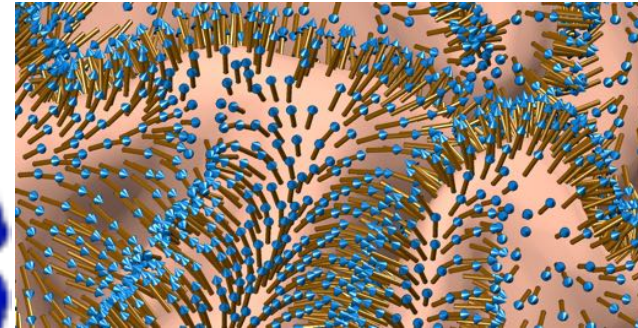
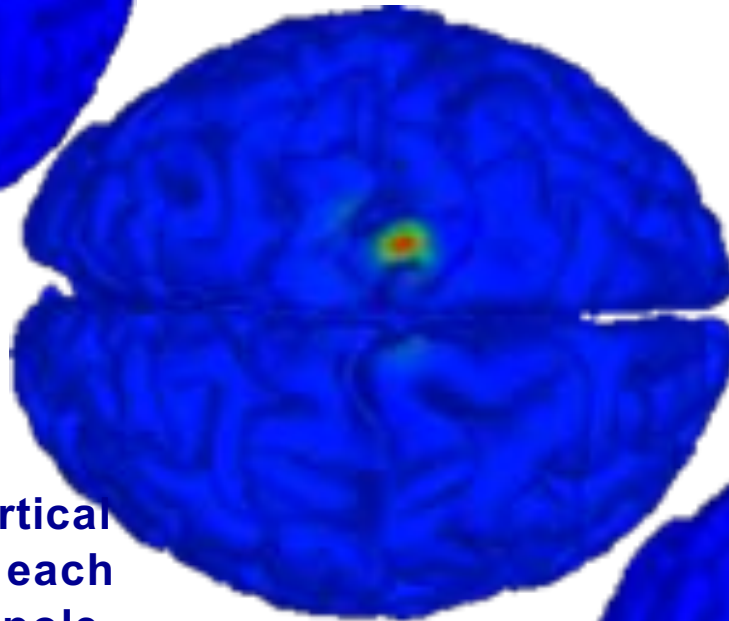
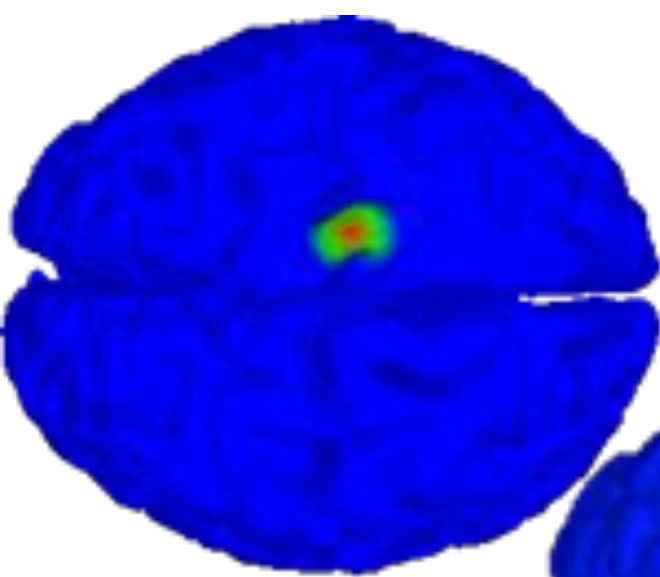
**Arthur Tsai –
Topological
source clustering
and
measure projection**



Arthur Tsai et al., *NeuroImage*, 2014

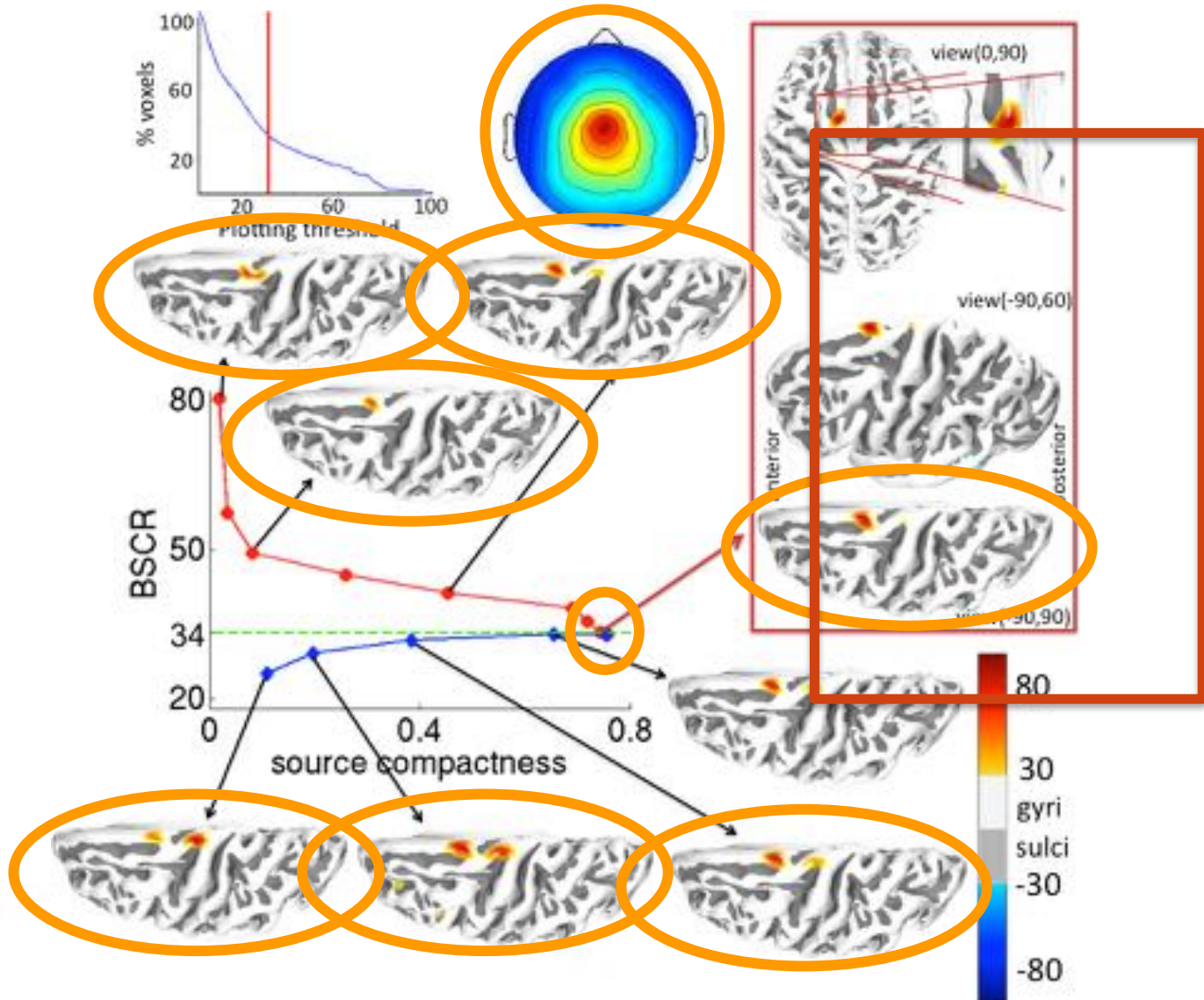
High-Resolution Distributed Source Localization

using a multiscale patch basis



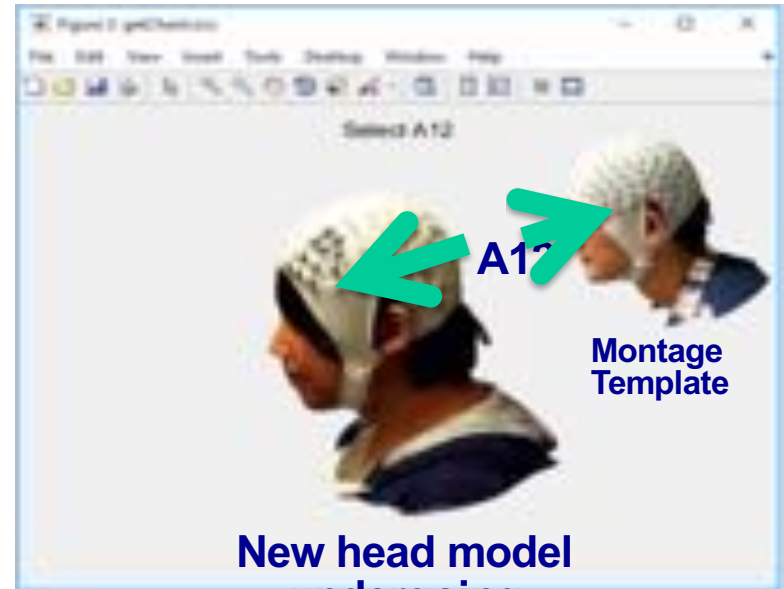
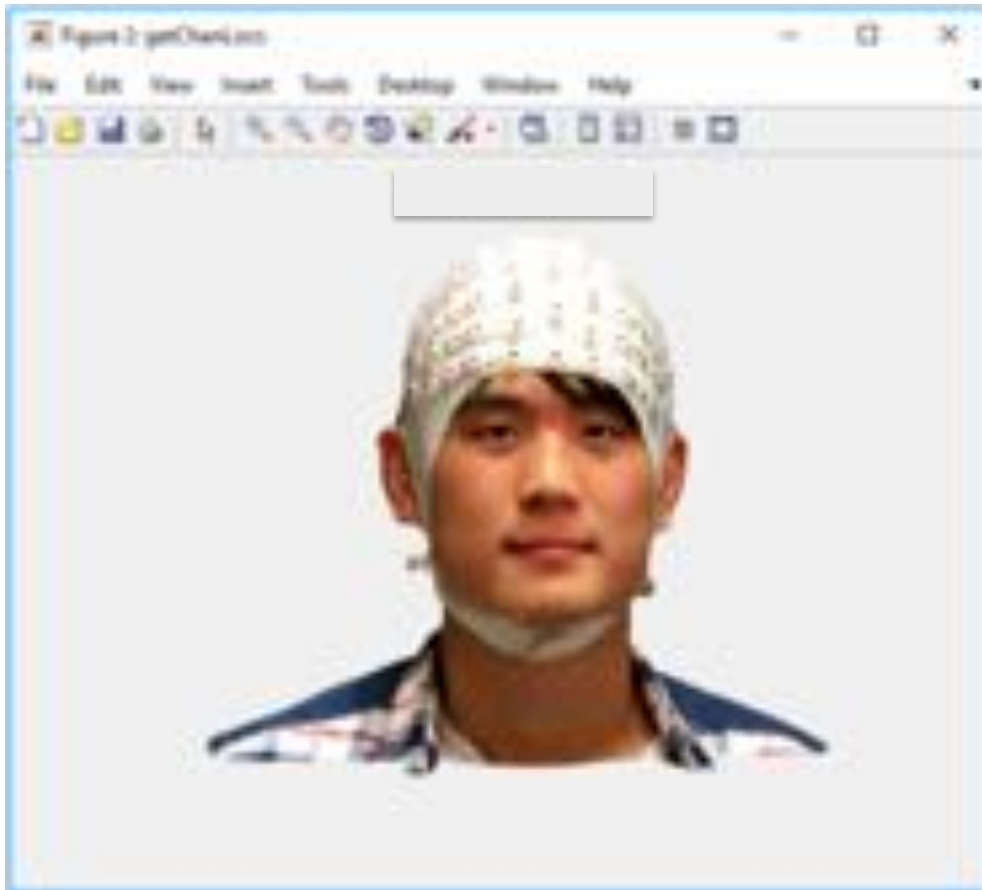
0. Build a high-res. cortical surface mesh; give each voxel an oriented dipole.
1. Compute a 'dictionary' of Gaussian patches conforming to the cortical surface centered at each cortical mesh voxel.
2. Use a 'sparsifying' approach to find the sum of the *fewest* of these patches that together produce the given source scalp or grid map.

High-resolution source localization requires an *electrically* accurate head model



Handheld 3-D electrode position recording system software

sccn.ucsd.edu/wiki/Get_chanlocs



**New head model
undergoing
electrode
localization**

**Currently by hand 1-by-1.
Soon by machine learning.**

Brain imaging during movement – How?

- Current advances in miniaturization, computer power, and information-based signal processing make possible a new imaging modality:

Mobile

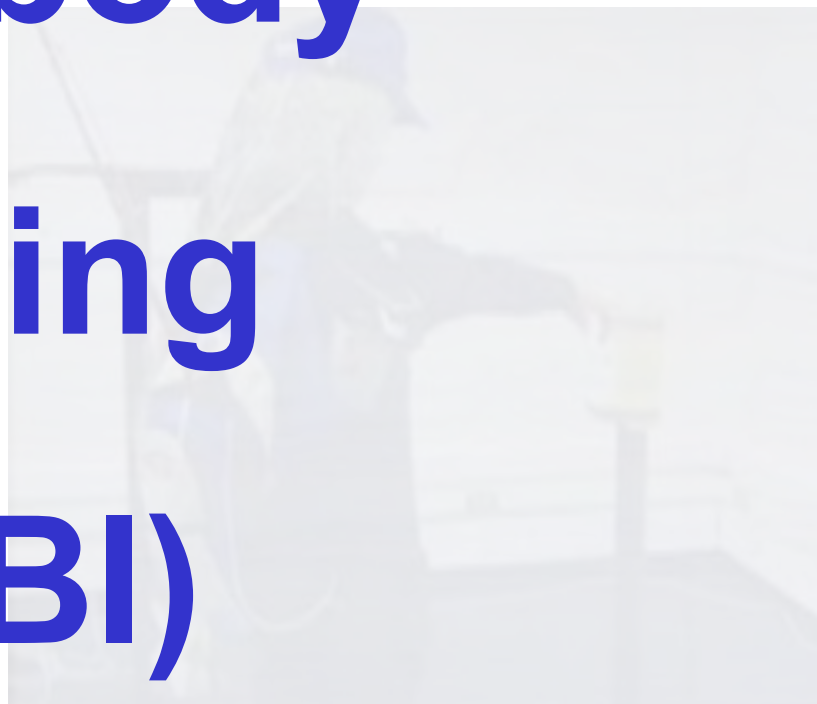
→ **Mobile Brain/Body Imaging (MoBI)**

Brain/body

Concept:

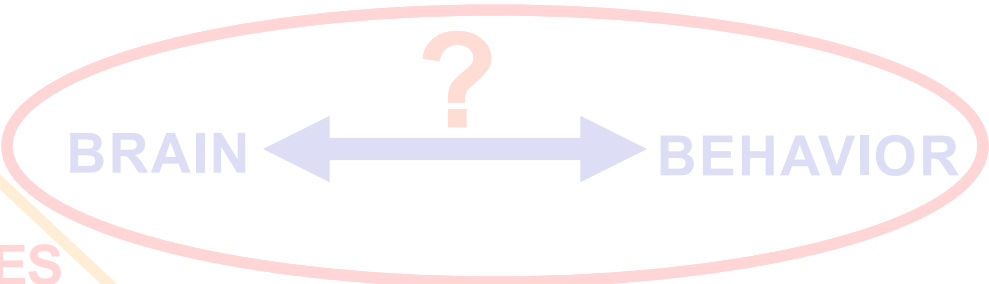
Combine whole-head cEEG, eye gaze tracking, and whole-body motion capture recording in a real-world 3-D environment.

Imaging (MoBI)



M
I
C
R
O

M
O
B
I



SPIKES

LFP

ECOG

Recorded !?

Average

RT

~1 Hz

~1,000,000 GHz

Mobile Brain/Body Imaging

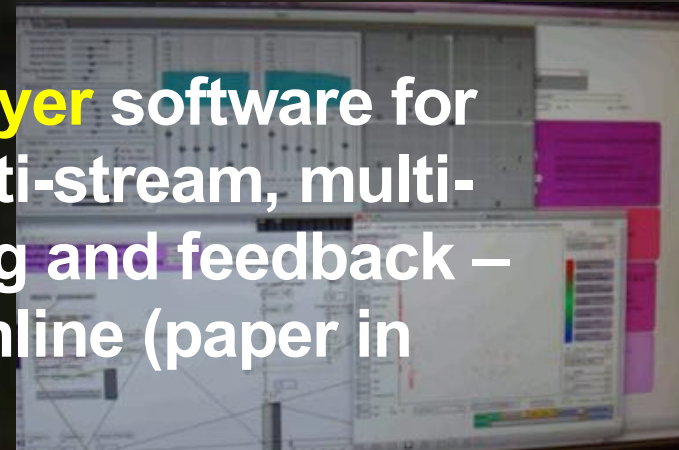
Record what the brain does,
What the brain experiences,
And what the brain
organizes.

MoBI Lab at SCCN, UCSD



Lab Streaming Layer software for synchronous multi-stream, multi-platform recording and feedback – freely available online (paper in progress):

github.com/labstreaminglayer



Extensible Data Format (xdf) for multimodal data collection and storage.

SNAP – a python-based framework running on Unity for control of simple or complex MoBI experiments.

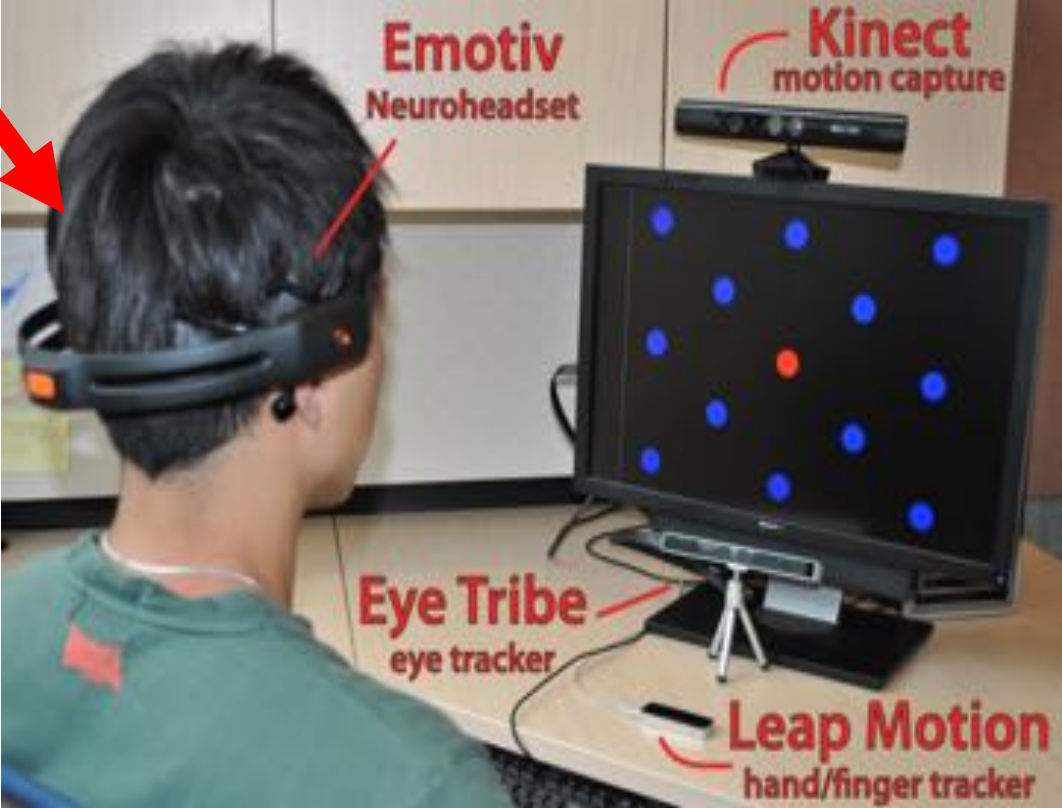
MoBILAB – a Matlab-based multimodal data browser and pre-processing app.



Now feasible – Low-cost MoBI Systems

Any EEG System →

Low-Cost MoBI



< \$500 Emotiv Neuroheadset

< \$500 Kinect motion capture

< \$500 Touchscreen

< \$1000 Full Body Wireless Inertial Motion Capture

< \$100 Eye Tribe eye tracker

< \$100 Leap Motion hand/finger tracker

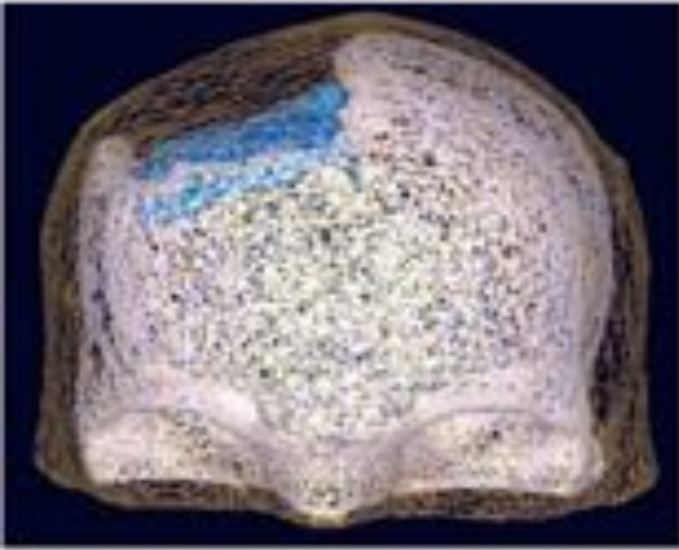
LSL software drivers exist for all these (and more) devices

A photograph of a man in a white lab coat and a red tie, smiling and shaking hands with another person. The image is framed by a red border. The text 'Imaging Human Agency and Social Interactions' is overlaid in red on the center of the image.

**Imaging Human Agency
and Social Interactions**



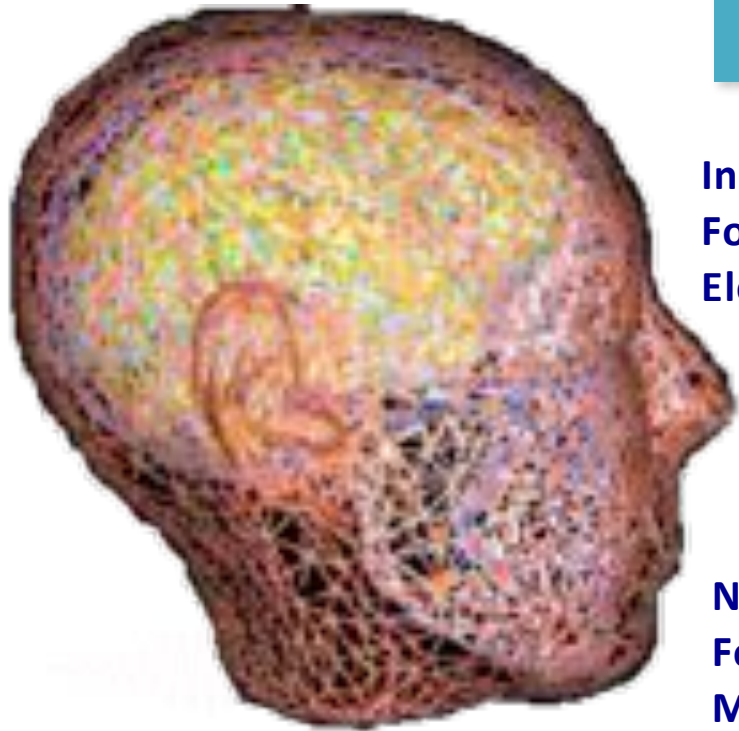
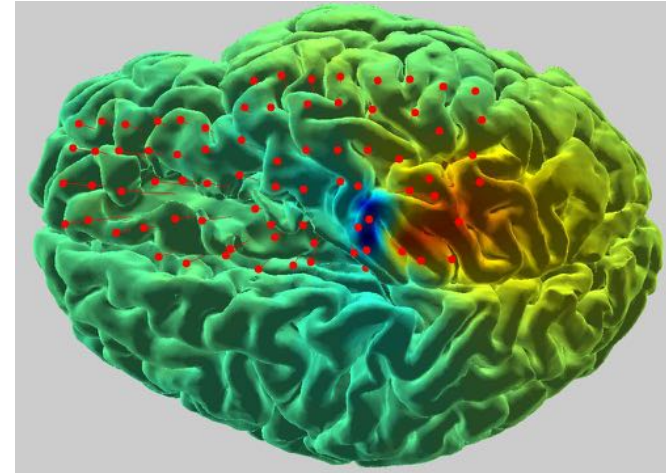
ECoG Source Analysis



**Invasively
Monitored Head --
Forward Electrical
Model**

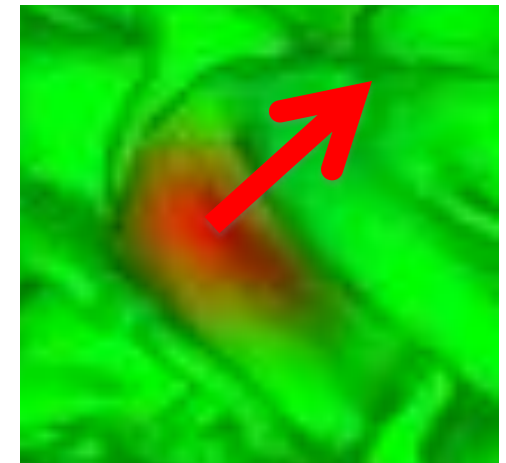
**Electrical
Brain Source
Analysis
for
ECoG**

**Independent
Component Source of
ECoG Data**

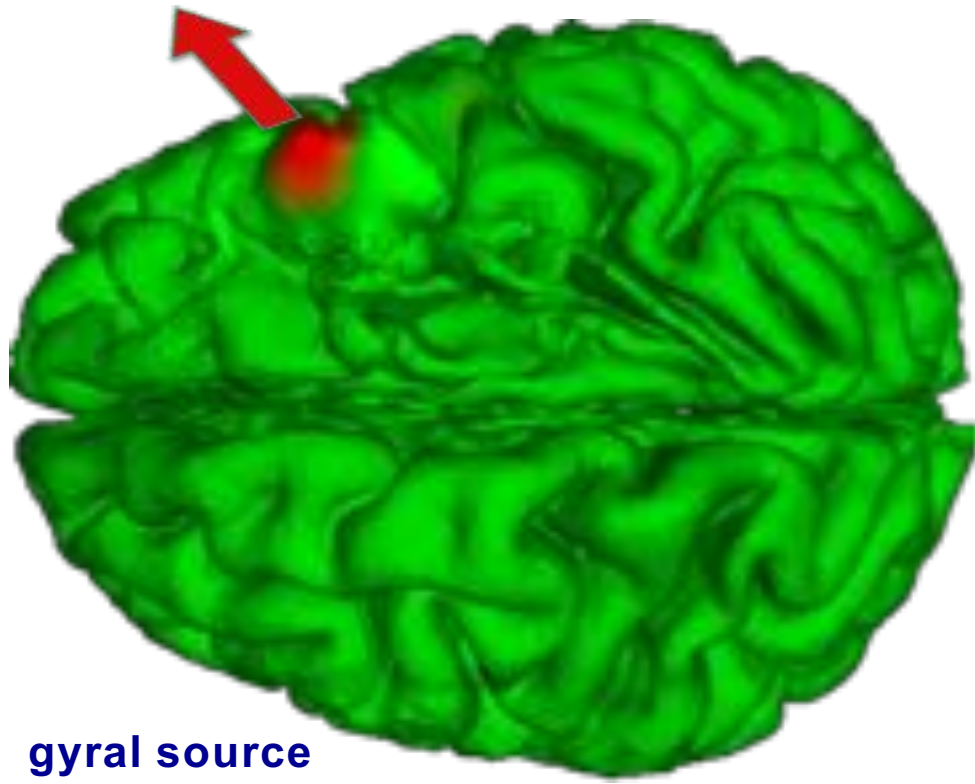


**Intact Head --
Forward
Electrical Model**

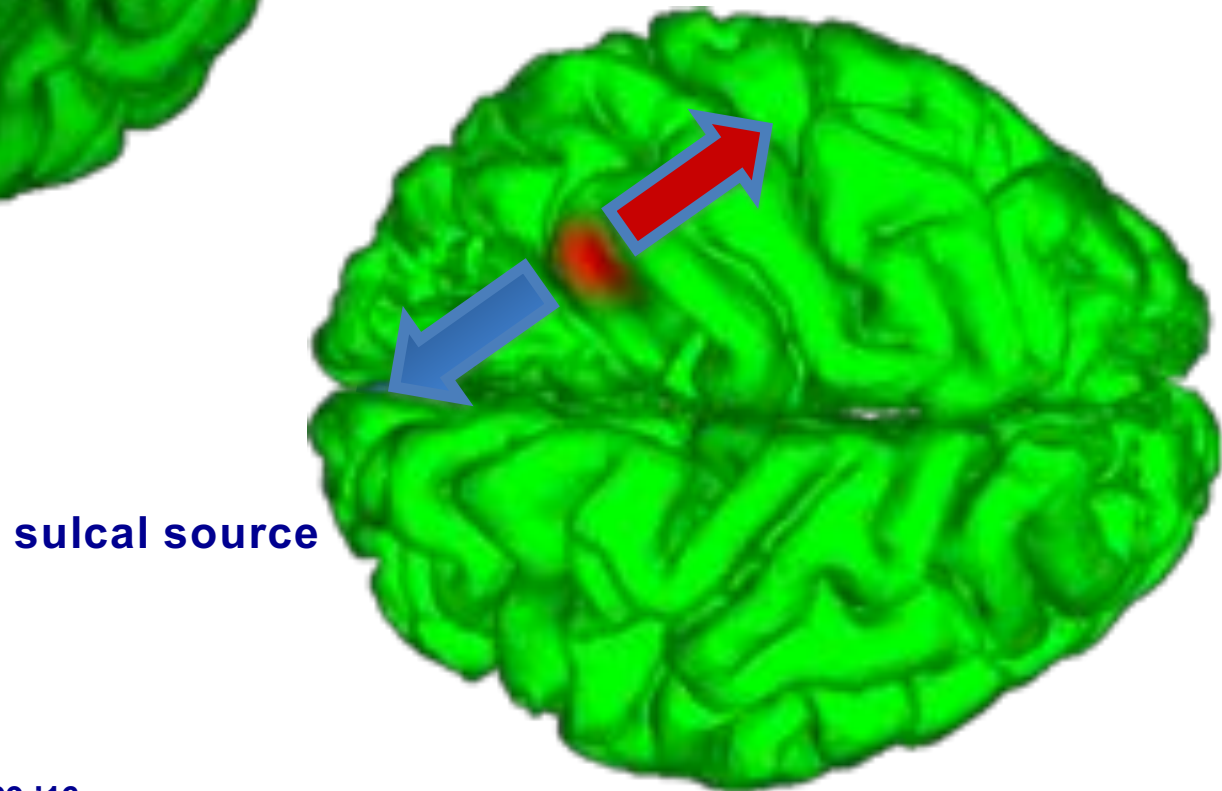
**Neuroelectromagnetic
Forward Head
Modeling Toolbox
(NFT)**



**Source Patch in Sulcus
Estimated using the
Forward Head Model**



ECoG Data Source Decomposition by ICA



Just as, currently, MRI & fMRI signals are only interpreted after transformation from sensor space to *brain source space*,

So too, in future, electrophysiological signals should (and will) be interpreted only after suitable transformation from EEG|ECoG|LFP sensor space to *brain effective source space*.

→ The dependence on spatially stable source dynamics forced by ICA is artificial; more general models of spatiotemporal field trajectories (e.g., using deconvolutive ICA or complex ICA).